The atypical cation-conduction and gating properties of ELIC underscore the marked functional versatility of the pentameric ligand-gated ion-channel fold

Giovanni Gonzalez-Gutierrez1 and Claudio Grosman1,2,3

1Department of Molecular and Integrative Physiology, 2Center for Biophysics and Computational Biology, and 3Neuroscience Program, University of Illinois at Urbana-Champaign, Urbana, IL 61801

The superfamily of pentameric ligand-gated ion channels (pLGICs) is unique among ionotropic receptors in that the same overall structure has evolved to generate multiple members with different combinations of agonist specificities and permeant-ion charge selectivities. However, aside from these differences, pLGICs have been typically regarded as having several invariant functional properties. These include pore blockade by extracellular quaternary-ammonium cations in the micromolar-to-millimolar concentration range (in the case of the cation-selective members), and a gain-of-function phenotype, which manifests as a slower deactivation time course, as a result of mutations that reduce the hydrophobicity of the transmembrane pore lining. Here, we tested this notion on three distantly related cation-selective members of the pLGIC superfamily: the mouse muscle nicotinic acetylcholine receptor (nAChR), and the bacterial GLIC and ELIC channels. Remarkably, we found that, whereas low millimolar concentrations of TMA+ and TEA+ block the nAChR and GLIC, neither of these two quaternary-ammonium cations blocks ELIC at such concentrations; instead, both carry measurable inward currents when present as the only cations on the extracellular side. Also, we found that, whereas lidocaine binding speeds up the current-decay time courses of the nAChR and GLIC in the presence of saturating concentrations of agonists, the binding of lidocaine to ELIC slows this time course down. Furthermore, whereas mutations that reduce the hydrophobicity of the side chains at position 9 of the M2 α-helices greatly slowed the deactivation time course of the nAChR and GLIC, these mutations had little effect—or even sped up deactivation—when engineered in ELIC. Our data indicate that caution should be exercised when generalizing results obtained with ELIC to the rest of the pLGICs, but more intriguingly, they hint at the possibility that ELIC is a representative of a novel branch of the superfamily with markedly divergent pore properties despite a well-conserved three-dimensional architecture.

INTRODUCTION

Structure–function studies of bacterial pentameric ligand-gated ion channels (pLGICs) have led to the notion that both structure and function are remarkably well-conserved in the superfamily despite little amino acid sequence conservation. Indeed, even in the absence of the eponymous cysteine loop or the long intracellular linker between the M3 and M4 transmembrane α-helices, the bacterial members studied thus far open and desensitize upon binding extracellular ligands, much like their homologues from the nervous system of animals (Bocquet et al., 2007; Gonzalez-Gutierrez and Grosman, 2010; Parikh et al., 2011; Zimmermann and Dutzler, 2011; Gonzalez-Gutierrez et al., 2012).

From studies performed largely on the animal members of the superfamily, it has been concluded that—aside from being activated by different ligands and having opposite charge selectivities—pLGICs form a group of ion channels that share several functional properties. For example: (a) the transmembrane pore of the cation-selective members is blocked by extracellular quaternary-ammonium cations in the micromolar-to-millimolar concentration range (Neher and Steinbach, 1978; Adler et al., 1979; Sine and Steinbach, 1984; Ogden and Colquhoun, 1985; Marshall et al., 1990; Cuevas and Adams, 1994; Zhang et al., 1995; Blanchet and Dulon, 2001; Akk and Steinbach, 2003; Purohit and Grosman, 2006), discriminates poorly among monovalent cations (Adams et al., 1980; Yang, 1990), and displays some permeability to Ca2+ (Adams et al., 1980; Decker and Dani, 1990; Yang 1990; Zhou and Neher, 1993; Elenes et al., 2009); (b) the transmembrane pore of the anion-selective members is blocked by picrotoxin (Chang and Weiss, 1998, 1999; Etter et al., 1999; Sedelnikova et al., 2006; Bali and Akabas, 2007; Wang et al., 2007); (c) the rearrangement of the loop between the extracellular domain β-strands 9 and 10 (the C-loop) is an integral part of the...
conformational changes that occur upon ligand binding or gating (Chen et al., 1995; Hansen et al., 2005; Mukhtasimova et al., 2009; Hibbs and Gouaux, 2011; Purohit and Auerbach, 2013; Voluk et al., 2013); and (d) mutations that reduce the hydrophobicity of the transmembrane pore lining invariably lead to a gain-of-function phenotype (regardless of the channel’s charge selectivity) that results from a stabilized open-channel conformation and manifests, for example, as an increased sensitivity to agonists, an increased unliganded-gating activity, longer bursts and clusters of single-channel openings, a slower time course of deactivation, and a slower time course of desensitization (Revah et al., 1991; Filatov and White, 1995; Labarca et al., 1995; Kearney et al., 1996; Chang and Weiss, 1998, 1999; Thompson et al., 1999; Kosolapov et al., 2000; Bianchi and Macdonald, 2001; Cymes et al., 2002; Burzomato et al., 2003; Grosman, 2003; Shan et al., 2003; Cymes et al., 2005; Papke and Grosman, 2014). Importantly, the discovery of the more distantly related bacterial and archaeal pLGICs (Tasneem et al., 2005) has afforded us the possibility to challenge these concepts in the framework of an even more diverse group of homologues. Although it seems likely that all members of the superfamily—from bacterial and archaeal to human—form ion channels gated by extracellular ligands, the degree to which more detailed aspects of molecular function are conserved remains to be ascertained.

Not much is known about the relationship between structure and function in bacterial or archaeal pLGICs, but some intriguing differences have already begun to emerge. A case in point is the C-loop of the extracellular domain. Whereas mutations to this loop have been found to impair the activation of animal pLGICs profoundly (Chen et al., 1995; Shen et al., 2012), we have recently shown that the entire C-loop of the bacterial homologue ligand-gated ion channel from Gloeobacter violaceus (GLIC) can be deleted without compromising its function as a proton-gated channel (Gonzalez-Gutierrez et al., 2013). Another example is the atypical phenotype of leucine-to-alanine mutations at the pore-lining position 9 of the M2 transmembrane α-helix of ligand-gated ion channel from Erwinia chrysanthemi (ELIC; Gonzalez-Gutierrez et al., 2012), a finding that we investigate further here with additional mutations. Yet another example is the larger number of exponential components observed for the distribution of open times of ELIC recorded at saturating concentrations of agonist (propylamine) compared with the single component observed under comparable experimental conditions in the cases of the (animal) muscle nicotinic acetylcholine receptor (nAChR) and the α1 glycine receptor (Marabelli et al., 2015).

In this paper, we set out to study some of the properties of the transmembrane pore. We compared the effects of pore blockers (tetramethylammonium [TMA+], tetraethylammonium [TEA+], and lidocaine) and mutations to the pore’s hydrophobic lining on the function of three distantly related cation-selective members of the superfamily: the mouse muscle nAChR, and the bacterial GLIC and ELIC channels. Strikingly, we found that, whereas millimolar concentrations of extracellular TMA+ and TEA+ block the nAChR and GLIC, neither of these two quaternary-ammonium cations blocks ELIC at a concentration as high as 50 mM, and instead, both carry measurable inward currents when present as the only cations on the extracellular side. Also, we found that, whereas lidocaine binding speeds up the time course of the current decay of the nAChR and GLIC on sustained application of saturating concentrations of agonist, the binding of lidocaine to ELIC slows this time course down, and the crystal structure of the ELIC–lidocaine complex shows the anesthetic bound to the cavity lined by the back of the M2 and the front of the M1 and M3 transmembrane α-helices. In marked contrast, in both the nAChR (Leonard et al., 1988; Charnet et al., 1990) and GLIC (Hilf et al., 2010), lidocaine (or its trimethyl-ammonium counterpart, QX-222) has been found to bind to the transmembrane pore, i.e., the cavity lined by the front side of the five M2 α-helices. Finally, whereas mutations that reduce the hydrophobicity of the pore-lining side chains greatly slowed down the time course of deactivation of the nAChR and GLIC—a phenomenon often regarded as a hallmark of the entire superfamily—we found that these mutations have little or even the opposite effect when engineered in ELIC.

MATERIALS AND METHODS

cDNA clones, mutagenesis, and heterologous expression
HEK-293 cells were transiently transfected with wild-type or mutant complementary DNAs (cDNAs) coding the mouse muscle adult-type nAChR (α1, β1, δ, and ε subunits), GLIC or ELIC using the calcium-phosphate precipitation method. nAChR cDNAs in the expression vector pRBG4 were provided by S. Sine (Mayo Clinic, Rochester, MN). GLIC and ELIC cDNAs in the pcDNA 3.1(−) vector (Life Technologies) were prepared as described previously (Gonzalez-Gutierrez and Grosman, 2010; Gonzalez-Gutierrez et al., 2012). For the calculation of identities and similarities between pairs of amino acid sequences, the number of identical or similar residues was divided by the average number of total residues in the two aligned sequences. Point mutations were engineered using the QuikChange site-directed mutagenesis kit (Agilent Technologies) and were confirmed by dideoxy sequencing.

Electrophysiological recordings and analysis
Ensemble (macroscopic) currents were recorded from transfected HEK-293 cells using the outside-out configuration of the patchclamp technique, whereas single-channel currents were recorded using either the outside-out or the cell-attached configuration, at ~22°C. For outside-out recordings, the ligand was applied to the external aspect of excised patches as rapid jumps (solution-exchange time τ = 0.005 < 150 µs). These step-changes in the concentration of ligand were achieved by the rapid switching of two solutions flowing from either barrel of a piece of theta-type
capillary glass mounted on a piezo-electric device (Burleigh-LSS-5100; discontinued). For all outside-out recordings, the patch-pipette solution consisted of (in mM) 142 KCl, 1.5 CaCl₂, 1.7 MgCl₂, 10 HEPES/KOH, pH 7.4; the solutions flowing through the two barrels of the perfusion tubing differed among experiments and are indicated in the text. For cell-attached recordings, the pipette solution consisted of (in mM) 140 KCl, 1.8 CaCl₂, 1.7 MgCl₂, 10 HEPES/KOH, pH 7.4, and the indicated agonist. The effective bandwidth for data analysis was DC–5 kHz for both macroscopic and single-channel currents. For display purposes, the macroscopic current traces were decimated, and the single-channel traces were filtered such that the cut-off frequency was 2–5 kHz. Both macroscopic and single-channel current recordings were analyzed using pClamp 9.0 (MDS Analytical Technologies).

To determine the effects of quaternary-amonium cations and lidocaine on the values of macroscopic peak currents and decay time constants of the muscle nAChR and GLIC, we used paired experiments. In these, the response of each patch of membrane to a pulse of agonist was recorded sequentially in the absence, in the presence, and back again in the absence (that is, upon washout) of the compound under study with the goal of reducing the impact of the variability from patch to patch. Thus, each patch acted as its own control and generated a value for the effect of each added compound. These values (obtained from several patches) were averaged, and the corresponding mean and standard error are presented in the form of bar graphs throughout the paper as normalized peak currents and normalized time constants. In the case of ELIC, however, paired experiments proved difficult because the channel activity usually ran down as a function of time after patch excision. Therefore, to maximize the amount of data obtained from each patch, the number of maneuvers within each single experiment was kept to a minimum. Thus, responses in the presence and in the absence of the tested compounds were recorded from separate (i.e., unpaired) patches of membrane. The ratios between the means of these values were calculated, and their corresponding standard errors were propagated; it is these values of ELIC that are presented in the form of bar graphs throughout the paper.

Because of the slow desensitization time courses of wild-type GLIC and ELIC (with time constants, in some patches, as slow as 8 s), the agonist typically had to be applied for long intervals (~1 min) for the currents to reach steady state, and hence, for accurate estimates of the exponential decay time constants to be obtained. These intervals proved to be too long, however, considering the average lifetime of a fast-perfused outside-out patch, on the one hand, and the multiple solution changes and consecutive agonist applications that we intended to perform on any given patch, on the other. Therefore, as a compromise, we applied 1-min pulses of agonist to only a few patches per tested condition and estimated the steady-state value of the current relative to the peak. With this information, we then proceeded to fix the steady-state current of fits to responses to shorter applications of agonist (5 s). In all cases, the steady-state values of the macroscopic currents on sustained application of agonist turned out to be nearly zero.

In an attempt to assess the statistical significance of the differences between the mean values of current decay time constants obtained under different conditions, we performed Student’s t-tests (paired or unpaired, depending on the experimental design) and report the corresponding two-tailed p-values.

**Protein purification, crystallization, and x-ray diffraction**

ELIC was purified as described in previous work (Gonzalez-Gutierrez et al., 2012). Concentrated protein (~10 mg/ml) was mixed with cysteamine (final concentration = 10 mM), *E. coli* total polar lipids (Avanti Polar; final concentration = 0.5 mg/ml), and lidocaine (final concentration = 15 mM) and the bromo derivative N1-(4-bromophenyl)-N2,N2-diethyl glycinalamide (Chembridge; final concentration = 15 mM). The protein was crystallized by vapor diffusion in hanging drops at 4°C. The reservoir solution consisted of 200 mM (NH₄)₂SO₄, 10–12% (wt/vol) PEG 4000 and 50 mM N-(2-acetamido) iminoacetic acid/NaOH, pH 6.5–6.7. For cryoprotection, crystals were transferred for a few seconds into reservoir solution supplemented with 30% (vol/vol) ethylene-glycol and were subsequently flash frozen in liquid nitrogen. Diffraction data were collected at 100 K at the 21-ID-D/F/G beamline at the Advanced Photon Source (Argonne National Laboratory, Argonne, IL). The data were indexed, integrated, and scaled using HKL2000 (Otwinowski and Minor, 1997). The structures were solved by molecular replacement using PDB deposition 2VLO as the search model. The Auto Build function in PHENIX (Adams et al., 2010) was used to generate a first model that was subsequently refined in PHENIX and Coot (Emsley et al., 2010). No attempts were made to refine regions of poor electron density as defined in the starting model. Cross-validation used 5% of the data in the calculation of the R-value. PyMOL was used to prepare molecular images (The PyMOL Molecular Graphics System, Version 1.3; Schrödinger). The model of ELIC was solved in the presence of cysteamine and lidocaine to a resolution of 3.65 Å; the wavelength used was 0.97872 Å. Because only a weak density for lidocaine was observed, a second structure in the presence of cysteamine and the bromo derivative N1-(4-bromophenyl)-N2,N2-diethyl glycinalamide was also solved (to a resolution of 4.23 Å). To confirm the presence of the heavy atom, a third dataset was obtained using a wavelength of 0.91838 Å (solved to a resolution of 4.82 Å).

**RESULTS**

Effects of quaternary-amonium cations and lidocaine on the nAChR and GLIC

To gain insight into the extent to which concepts derived from the study of the bacterial homologues of the pLGIC superfamily can be applied to their animal counterparts, we decided to compare some of their functional properties. We started by testing the effects of TEA’ and lidocaine on the (heteromeric) adult-type nAChR from mouse muscle, and the (homomeric) GLIC and ELIC channels from bacteria. Averaging the four types of subunit, the amino acid sequence of this nAChR is 16.7% identical (25.4% similar) to that of GLIC and 14.7% identical (23.1% similar) to that of ELIC. The amino acid sequence of GLIC is 20.4% identical (35.2% similar) to that of ELIC. Disregarding the highly variable M3–M4 linker, these values become 19.0% (identity) and 33.0% (similarity) for the muscle AChR and GLIC; 16.9% (identity) and 30.4% (similarity) for the muscle AChR and ELIC; and 20.5% (identity) and 35.8% (similarity) for GLIC and ELIC.

TEA’ applied to the extracellular side of outside-out patches at a concentration of 0.5–5.0 mM reduced the peak amplitude of the macroscopic currents flowing through the nAChR and GLIC with little (if any) effect on their time constants of desensitization (Figs. 1 and 2, and Table 1). The lower peak values of the nAChR-mediated macroscopic currents can be attributed to a
The atypical conduction and gating properties of ELIC amplitude yet slow enough for the individual blocking events to be discernible as sojourns in the zero-current level. Although analogous recordings from GLIC were not clear enough to draw meaningful conclusions (owing to the low single-channel conductance of this bacterial channel even in the absence of TEA+), we surmise that the effect of this organic cation on GLIC is essentially the same. Regarding desensitization of these two channels, we would like to highlight the observation that the presence of blocking concentrations of TEA+ did not affect their time courses. Thus, the presence of a blocker inside the pore of a pLGIC’s crystal structure, for example, should not be taken to imply

Figure 1. Block of the muscle nAChR by TEA+. (A) Macroscopic current responses to 2-s pulses of 100 μM ACh recorded at −80 mV from the mouse muscle adult-type nAChR in the outside-out configuration. The response of each patch of membrane was recorded sequentially in the absence of TEA+ (left), in the presence of 0.5 mM TEA+ flowing through both barrels of the theta-type perfusion tubing (middle), and back again, without TEA+ in either barrel (right). The solutions flowing through the two barrels of the perfusion tubing were (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl2, 1.7 MgCl2, and 10 HEPES/KOH, pH 7.4 with or without ACh and with or without TEA+. In the schematic representations of the theta-tubing perfusion, arrows indicate the application of TEA+. Note the expanded current scale used for the middle panel; the trace is the average of 25 consecutive responses recorded from a representative patch. (B) Single-channel inward currents elicited by 100 μM ACh recorded in the presence or absence of 0.5 mM TEA+ at approximately −80 mV in the cell-attached configuration; openings are downward deflections. The pipette solution was (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl2, 1.7 MgCl2, 0.1 ACh, and 10 HEPES/KOH, pH 7.4 with or without TEA+. (C) Peak-current amplitudes recorded in response to the application of ACh in the presence of external 0.5 mM or 5.0 mM TEA+ and upon TEA+ removal normalized to the peak value observed in the initial TEA+-free recording. (D) Time constants of desensitization during the application of ACh in the presence of 0.5 mM or 5.0 mM TEA+ and upon TEA+ removal normalized to the time constant fitted to the initial TEA+-free recording. The values plotted in C and D are means obtained from 6 patches; error bars are the corresponding standard errors.

Figure 2. Block of GLIC by TEA+. (A) Macroscopic current responses to 5-s pulses of pH 4.5 solution (pHholding 7.4) recorded at −80 mV in the outside-out configuration. The response of each patch of membrane was recorded sequentially in the absence of TEA+ (left), in the presence of 5 mM TEA+ flowing through both barrels of the theta-type perfusion tubing (middle), and back again, without TEA+ in either barrel (right). The solutions flowing through the two barrels of the perfusion tubing were (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl2, 1.7 MgCl2 with or without TEA+, and pH buffered with 10 mM HEPES/KOH, pH 7.4, or with 10 mM acetic acid/KOH, pH 4.5. In the schematic representations of the theta-tubing perfusion, arrows indicate the application of TEA+. Note the expanded current scale used for the middle panel; the trace is the average of 25 consecutive responses recorded from a representative patch. (B) Peak-current amplitudes recorded in response to the application of pH 4.5 in the presence of external 5 mM TEA+ and upon TEA+ removal normalized to the peak value observed in the initial TEA+-free recording. (C) Time constants of desensitization during the application of pH 4.5 in the presence of external 5 mM TEA+ and upon TEA+ removal normalized to the time constant fitted to the initial TEA+-free recording. The values plotted in B and C are means obtained from 6 patches; error bars are the corresponding standard errors.
that the crystallized conformation represents the open state because pore block (at least by TEA⁺) does not prevent channel desensitization.

Extracellular lidocaine also reduced the peak currents mediated by the nAChR (Fig. 3, A and B), but unlike TEA⁺, this local anesthetic sped up the time course of current decay by a factor of ~100 (Fig. 3 C and Table 1). The lower peak values of the nAChR-mediated macroscopic currents can be attributed to the dramatically reduced single-channel open probability elicited by 100-µM ACh in the presence of 0.5 mM lidocaine (Fig. 3 A, insets). Because lidocaine is a slower blocker of the nAChR than is TEA⁺ (note that, in the presence of lidocaine, the amplitude of the single-channel currents remained essentially unaltered), it may be asked whether the faster decay of the macroscopic currents reflects faster desensitization or merely the kinetics of lidocaine entry into the open-channel pore. To learn more about the effect of lidocaine, we coapplied it with ACh for short intervals (Fig. 3 D). If lidocaine acted as a fast-dissociating open-channel blocker that does not alter the kinetics of closed–open–desensitized state interconversions, for example, the current upon washout of both lidocaine and ACh would be expected to rebound and attain the same value as that observed at the end of ACh-only pulses. This is not what we observed, however. Upon lidocaine and ACh washout, the signal remained close to the zero-current baseline (Fig. 3 D, vertical dashed line), a finding that is entirely consistent with lidocaine strongly biasing the channel’s conformational landscape toward a nonconductive conformation (such as the desensitized state). However, it may be

argued that this finding is also consistent with lidocaine dissociating slowly from the open-channel pore. As a result, we do not refer to this particular current decay time course as the time course of desensitization. Clearly, more experiments would be needed to elucidate the relative contributions of pore block and entry into desensitization to the current decay time course of the nAChR in the presence of both ACh and lidocaine. Obtaining such mechanistic insight was beyond the scope of this paper, however.

In the case of GLIC, the effect of extracellular 0.5 mM lidocaine on the macroscopic currents was qualitatively the same as that on the nAChR. Indeed, the peak currents were decreased to a large extent (Fig. 4, A and B), and the current-decay time course on continuous exposure to pH 4.5 extracellular solution was sped up, although in this case, only by a factor of ~3 (Fig. 4 C and Table 1). In fact, the ranges of time constant values of GLIC with and without lidocaine overlapped partially (Table 1), but the application of lidocaine to each individual patch (as illustrated in Fig. 4 A) sped up the time course of current decay in all 12 tested patches. The time constant fitted to each patch varied widely from patch to patch, but its value always became faster upon adding lidocaine (and thus, we cannot explain the slowing effect reported by Velisetty and Chakrapani (2012) for lidocaine on the current-decay time course of GLIC). Again, although single-channel recordings from GLIC in the presence of lidocaine were not clear enough to draw conclusions, it seems likely that this local anesthetic also lowers the channel’s open probability, much like it does on the nAChR.

<table>
<thead>
<tr>
<th>Channel</th>
<th>Conditions</th>
<th>( \tau_{\text{decay}} ) (mean ± SE; ms)</th>
<th>( \tau_{\text{decay}} ) (range; ms)</th>
<th>P-value</th>
<th>Number of patches</th>
</tr>
</thead>
<tbody>
<tr>
<td>Wild-type nAChR</td>
<td>Control</td>
<td>37.0 ± 8.8</td>
<td>16.7–63.7</td>
<td>0.37</td>
<td>6</td>
</tr>
<tr>
<td></td>
<td>0.5 mM TEA⁺</td>
<td>41.2 ± 10.5</td>
<td>23.9–74.6</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Wild-type nAChR</td>
<td>Control</td>
<td>48.9 ± 6.8</td>
<td>22.8–61.9</td>
<td>0.11</td>
<td>6</td>
</tr>
<tr>
<td></td>
<td>5 mM TEA⁺</td>
<td>59.5 ± 5.5</td>
<td>42.3–73.8</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Wild-type nAChR</td>
<td>Control</td>
<td>59.8 ± 3.7</td>
<td>51.9–67.1</td>
<td>7.6 × 10⁻⁷</td>
<td>4</td>
</tr>
<tr>
<td></td>
<td>0.5 mM lidocaine</td>
<td>0.60 ± 0.07</td>
<td>0.45–0.71</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Wild-type GLIC</td>
<td>Control</td>
<td>2.197 ± 950</td>
<td>154–3,928</td>
<td>0.34</td>
<td>6</td>
</tr>
<tr>
<td>Wild-type GLIC</td>
<td>5 mM TEA⁺</td>
<td>1.749 ± 737</td>
<td>146–4,057</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Wild-type GLIC</td>
<td>Control</td>
<td>2.072 ± 452</td>
<td>105–5,360</td>
<td>4.3 × 10⁻³</td>
<td>12</td>
</tr>
<tr>
<td>Wild-type GLIC</td>
<td>0.5 mM lidocaine</td>
<td>698 ± 208</td>
<td>36.7–2,045</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Wild-type ELIC</td>
<td>Control</td>
<td>4,533 ± 584</td>
<td>2,307–8,026</td>
<td>–</td>
<td>9</td>
</tr>
<tr>
<td></td>
<td>50 mM TEA⁺</td>
<td>5,353 ± 988</td>
<td>2,443–10,324</td>
<td>0.22</td>
<td>8</td>
</tr>
<tr>
<td>Wild-type ELIC</td>
<td>5 mM TEA⁺ (pipette)</td>
<td>5,370 ± 531</td>
<td>3,979–6,677</td>
<td>0.16</td>
<td>5</td>
</tr>
<tr>
<td></td>
<td>5 mM lidocaine</td>
<td>unmeasurably slow</td>
<td>–</td>
<td>–</td>
<td>14</td>
</tr>
<tr>
<td></td>
<td>50 mM TMA⁺</td>
<td>4,726 ± 782</td>
<td>1,608–7,725</td>
<td>0.84</td>
<td>9</td>
</tr>
<tr>
<td>L9‘A + F16‘L ELIC</td>
<td>Control</td>
<td>unmeasurably slow</td>
<td>–</td>
<td>–</td>
<td>17</td>
</tr>
<tr>
<td></td>
<td>50 mM TEA⁺</td>
<td>unmeasurably slow</td>
<td>–</td>
<td>–</td>
<td>7</td>
</tr>
<tr>
<td></td>
<td>50 mM TMA⁺</td>
<td>unmeasurably slow</td>
<td>–</td>
<td>–</td>
<td>11</td>
</tr>
</tbody>
</table>
20 The atypical conduction and gating properties of ELIC

Figure 3. Block of the muscle nAChR by lidocaine. (A) Macroscopic current responses to 2-s pulses of 100 µM ACh recorded at –80 mV from the mouse muscle adult-type nAChR in the outside-out configuration. The response of each patch of membrane was recorded sequentially in the absence of lidocaine (left), in the presence of 0.5 mM lidocaine flowing through both barrels of the theta-type perfusion tubing (middle), and back again, without lidocaine in either barrel (right). The insets show the much lower open probability of the channel in the presence of 0.5 mM external lidocaine; openings are downward deflections. The solutions flowing through the two barrels of the perfusion tubing were (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl₂, 1.7 MgCl₂, and 10 HEPES/KOH, pH 7.4 with or without ACh and with or without lidocaine. In the schematic representations of the theta-tubing perfusion, arrows indicate the application of lidocaine. Note the expanded current scale used for the middle panel; the trace is the average of 25 consecutive responses recorded from a representative patch. (B) Peak-current amplitudes recorded in response to the application of ACh in the presence of external 0.5 mM lidocaine and upon lidocaine removal normalized to the peak value observed in the initial lidocaine-free recording. (C) Current-decay time constants during the application of ACh in the presence of external 0.5 mM lidocaine and upon lidocaine removal normalized to the time constant fitted to the initial lidocaine-free recording. The values plotted in B and C are means obtained from 4 patches; error bars are the corresponding standard errors.

Figure 4. Block of GLIC by lidocaine. (A) Macroscopic current responses to 5-s pulses of pH-4.5 solution (pHholding 7.4) recorded at –80 mV in the outside-out configuration. The response of each patch of membrane was recorded sequentially in the absence of lidocaine (left), in the presence of 0.5 mM lidocaine flowing through both barrels of the theta-type perfusion tubing (middle), and back again, without lidocaine in either barrel (right). The solutions flowing through the two barrels of the perfusion tubing were (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl₂, 1.7 MgCl₂ with or without lidocaine, and pH-buffered with 10 mM HEPES/KOH, pH 7.4, or with 10 mM acetic-acid/KOH, pH 4.5. In the schematic representations of the theta-tubing perfusion, arrows indicate the application of lidocaine. Note the expanded current scale used for the middle panel; the trace is the average of 25 consecutive responses recorded from a representative patch. (B) Peak-current amplitudes recorded in response to the application of pH 4.5 in the presence of external 0.5 mM lidocaine and upon lidocaine removal normalized to the peak value observed in the initial lidocaine-free recording. (C) Current-decay time constants during the application of pH 4.5 in the presence of external 0.5 mM lidocaine and upon lidocaine removal normalized to the time constant fitted to the initial lidocaine-free recording. The values plotted in B and C are means obtained from 12 patches; error bars are the corresponding standard errors.
the presence of TEA$^+$ on either side of the membrane (Fig. 5 C and Table 1). Importantly, ELIC’s open probability between desensitized intervals in the presence of 10 mM cysteamine and the absence of TEA$^+$ is similar ($\approx 0.95$; Gonzalez-Gutierrez et al., 2012) to that of the muscle nAChR in the presence of 100-µM ACh and the absence of TEA$^+$ ($\approx 0.85$; Gonzalez-Gutierrez and Grosman, 2010), and therefore, the possibility that a lower open probability in the absence of blocker underlies the much lower extent of block observed for ELIC can be completely ruled out.

Application of extracellular 5 mM lidocaine to ELIC, on the other hand, reduced the peak currents elicited by pulses of 10 mM cysteamine by a factor of $\approx 16$ (mean peak current in the absence of lidocaine = 466 ± 109 pA, $n = 16$ patches; mean peak current in the presence of lidocaine = 29 ± 8 pA, $n = 14$ patches), and single-channel recordings also revealed a markedly reduced open probability (Fig. 6, A and B). Note, however, that a concentration
The atypical conduction and gating properties of ELIC open-channel conformation of ELIC so as to be able to make a more direct comparison with the existing data on the binding of lidocaine (or its quaternary-ammonium derivatives) to the nAChR and GLIC (Leonard et al., 1988; Charnet et al., 1990; Hilf et al., 2010). It may well be that a given compound binds to different cavities of the channel in its different conformational states. Also, it is important to note that we have used lidocaine here only as a probe of structure–function relationships in a bacterial channel; our results should not be regarded as shedding light on the binding of anesthetics to their animal targets.

To probe the effect of structural perturbations to the lidocaine-binding site of ELIC, we engineered five single-point mutants (Y245A, Y248A, and T249A, in M2—corresponding to positions 14, 17, and 18—and D263A and I266A, in M3; amino-acid numbering system as in Gonzalez-Gutierrez et al. [2012]) and one double mutant (Y203A + Y204A, in M1), and recorded their responses to 5-s pulses of a saturating concentration of agonist (Fig. 8). Three of these (Y203A + Y204A, T18A, and D263A) failed to give rise to functional expression, I266A was wild-type-like (Table 3), and Y14A and Y17A displayed faster desensitization time courses (by factors of ~17 and ~12, respectively; Table 3) and lower open-channel conformation of ELIC so as to be able to make a more direct comparison with the existing data on the binding of lidocaine (or its quaternary-ammonium derivatives) to the nAChR and GLIC (Leonard et al., 1988; Charnet et al., 1990; Hilf et al., 2010). It may well be that a given compound binds to different cavities of the channel in its different conformational states. Also, it is important to note that we have used lidocaine here only as a probe of structure–function relationships in a bacterial channel; our results should not be regarded as shedding light on the binding of anesthetics to their animal targets.

To probe the effect of structural perturbations to the lidocaine-binding site of ELIC, we engineered five single-point mutants (Y245A, Y248A, and T249A, in M2—corresponding to positions 14, 17, and 18—and D263A and I266A, in M3; amino-acid numbering system as in Gonzalez-Gutierrez et al. [2012]) and one double mutant (Y203A + Y204A, in M1), and recorded their responses to 5-s pulses of a saturating concentration of agonist (Fig. 8). Three of these (Y203A + Y204A, T18A, and D263A) failed to give rise to functional expression, I266A was wild-type-like (Table 3), and Y14A and Y17A displayed faster desensitization time courses (by factors of ~17 and ~12, respectively; Table 3) and lower open-channel conformation of ELIC so as to be able to make a more direct comparison with the existing data on the binding of lidocaine (or its quaternary-ammonium derivatives) to the nAChR and GLIC (Leonard et al., 1988; Charnet et al., 1990; Hilf et al., 2010). It may well be that a given compound binds to different cavities of the channel in its different conformational states. Also, it is important to note that we have used lidocaine here only as a probe of structure–function relationships in a bacterial channel; our results should not be regarded as shedding light on the binding of anesthetics to their animal targets.
mediated by ELIC (Fig. 5, A and B). We reasoned that this lack of block could be the result of the open-channel pore of ELIC being too narrow to allow the access of a cation as large as TEA⁺ (\(6.9\) Å diam; Conway et al., 1966; Edward, 1970; Ue, 1994). Alternatively, at the other end of the spectrum of possibilities, the pore of ELIC in the open state could be wide enough and have the necessary electrostatic properties for TEA⁺ to permeate nearly as fast as the mixture of K⁺, Na⁺, Ca²⁺, and Mg²⁺ of our extracellular solution in such a way that the competition between TEA⁺ and these inorganic cations would not result in a decreased conductance.

To test the possibility that the extracellular entrance to the transmembrane pore of ELIC is simply too narrow, we mutated the leucines at position 9 and the phenylalanines at position 16 to alanines and leucines, respectively, in an attempt to widen the pore cavity. The side chains at these two positions project into the lumen of the channel pore in the crystallized nonconductive conformation of ELIC (Hilf and Dutzler, 2008) and are likely to also do so in the open-channel conformation; in the muscle nAChR, they certainly do (Cymes et al., 2005). As was the case for wild-type ELIC, however, neither the peak value of the macroscopic currents nor the time course of the current response recorded from the

<table>
<thead>
<tr>
<th>Data collection</th>
<th>ELIC + cysteamine + lidocaine</th>
<th>ELIC + cysteamine + brominated analog</th>
<th>ELIC + cysteamine + brominated analog</th>
</tr>
</thead>
<tbody>
<tr>
<td>Space group</td>
<td>P21</td>
<td>P21</td>
<td>P21</td>
</tr>
<tr>
<td>Wavelength (Å)</td>
<td>0.97872</td>
<td>0.97872</td>
<td>0.91838</td>
</tr>
<tr>
<td>a, b, c (Å)</td>
<td>104.96, 266.74, 110.60</td>
<td>105.58, 267.78, 110.43</td>
<td>105.89, 267.96, 110.29</td>
</tr>
<tr>
<td>α, β, γ (°)</td>
<td>90, 109.15, 90</td>
<td>90, 110.82, 90</td>
<td>90, 109.53, 90</td>
</tr>
<tr>
<td>Resolution (Å)</td>
<td>50–3.65 (3.78–3.65)</td>
<td>50–4.25 (4.38–4.23)</td>
<td>50–4.82 (4.99–4.82)</td>
</tr>
<tr>
<td>Rwp</td>
<td>0.125 (0.653)</td>
<td>0.112 (&gt;1.0)</td>
<td>0.103 (0.716)</td>
</tr>
<tr>
<td>Rexp</td>
<td>0.134 (0.745)</td>
<td>0.122 (&gt;1.0)</td>
<td>0.122 (0.856)</td>
</tr>
<tr>
<td>Rmerge</td>
<td>0.051 (0.348)</td>
<td>0.069 (0.989)</td>
<td>0.065 (0.472)</td>
</tr>
<tr>
<td>I/σ(I)</td>
<td>13.6 (1.6)</td>
<td>8.6 (1.2)</td>
<td>10.4 (1.1)</td>
</tr>
<tr>
<td>Completeness (%)</td>
<td>98.9 (77.9)</td>
<td>97.9 (96.7)</td>
<td>96.3 (94.0)</td>
</tr>
<tr>
<td>Multiplicity</td>
<td>6.8 (3.5)</td>
<td>5.9 (4.9)</td>
<td>3.4 (2.9)</td>
</tr>
</tbody>
</table>

Because pore block by extracellular quaternary-ammonium cations is one of the most characteristic properties of the cation-selective pLGICs, we were intrigued by our finding that 50 mM TEA⁺ did not block the currents mediated by ELIC (Fig. 5, A and B). We reasoned that this lack of block could be the result of the open-channel pore of ELIC being too narrow to allow the access of a cation as large as TEA⁺ (\(~6.9\) Å diam; Conway et al., 1966; Edward, 1970; Ue, 1994). Alternatively, at the other end of the spectrum of possibilities, the pore of ELIC in the open state could be wide enough and have the necessary electrostatic properties for TEA⁺ to permeate nearly as fast as the mixture of K⁺, Na⁺, Ca²⁺, and Mg²⁺ of our extracellular solution in such a way that the competition between TEA⁺ and these inorganic cations would not result in a decreased conductance.

To test the possibility that the extracellular entrance to the transmembrane pore of ELIC is simply too narrow, we mutated the leucines at position 9 and the phenylalanines at position 16 to alanines and leucines, respectively, in an attempt to widen the pore cavity. The side chains at these two positions project into the lumen of the channel pore in the crystallized nonconductive conformation of ELIC (Hilf and Dutzler, 2008) and are likely to also do so in the open-channel conformation; in the muscle nAChR, they certainly do (Cymes et al., 2005). As was the case for wild-type ELIC, however, neither the peak value of the macroscopic currents nor the time course of the current response recorded from the
The atypical conduction and gating properties of ELIC

The conduction and gating properties of ELIC were affected by the continuous presence of extracellular TEA⁺ at a concentration as high as 50 mM (Fig. 9, A and B; and Table 1). The same was the case for TMA⁺ (a smaller cation, ~5.7 Å diam; Conway et al., 1966; Edward, 1970; Ue, 1994) on both the wild-type and the L9'A + F16'L wider-pore mutant at a concentration of 50 mM (Fig. 9, C–E; and Table 1). To emphasize the atypical properties of ELIC, Fig. 10 illustrates the blocking effect of TMA⁺ on the nAChR at the macroscopic and single-channel levels when also applied to the extracellular side at a concentration of 50 mM. TMA⁺ is both a fast pore blocker and an agonist of the nAChR.

Regarding the open probability between desensitized intervals of the L9'A + F16'L mutant of ELIC in the presence of 10 mM cysteamine and the absence of quaternary-ammonium cations, we note that its value (~0.45; Gonzalez-Gutierrez et al., 2012) is lower than the muscle-nAChR's (~0.85 in the presence of 100-µM ACh and the absence of quaternary-ammonium cations; Gonzalez-Gutierrez and Grosman, 2010) only by a factor of ~1.9. In other words, although lower, this open probability is not low enough to account for the negligible block of this double mutant by 50 mM TEA⁺ or TMA⁺.

Quaternary-ammonium cations carry measurable currents through ELIC

To test the possibility that TMA⁺ can conduct measurable currents through ELIC, we replaced the extracellular mixture of K⁺, Na⁺, Ca²⁺, and Mg²⁺ present in the agonist-containing barrel of the theta-type tubing of our perfusion system with a solution containing TMA⁺ and agonist alone. More specifically, this solution consisted of (in mM) 142 TMACl, 10 cysteamine chloride, and 10 HEPES/KOH, pH 7.4.
10 HEPES/TMAOH, pH 7.4; the solution flowing through the other barrel of the theta tube (that is, the agonist-free solution) remained unchanged (in mM: 142 KCl, 5.4 NaCl, 1.8 CaCl₂, 1.7 MgCl₂, and 10 HEPES/KOH, pH 7.4). To allow for a comparison across channel types, we also applied this type of pulse protocols to the nAChR and GLIC. Because TMA⁺ is a high-efficacy agonist of the nAChR, no additional ligands were added to the TMA⁺-containing solution when assaying this channel. In the case of GLIC, the pH of the 142-mM TMA⁺ solution was buffered with 10 mM acetic acid (instead of HEPES), and its value was adjusted to 4.5 with TMAOH.

The responses of the nAChR and GLIC are illustrated in Fig. 11, whereas that of ELIC is illustrated in Fig. 12. In the case of the nAChR, the ratio between the macroscopic current values before and after TMA⁺ removal was ~0.08, thus suggesting that TMA⁺ carries a current that is ~8.0% of that carried by the mixture of K⁺, Na⁺, Ca²⁺, and Mg²⁺ present in the agonist-free solution (Fig. 11 A). Because the fast deactivation of the nAChR (time constant = 1.1 ± 0.1 ms; n = 12) could have led to an underestimation of the peak-value reached upon TMA⁺ removal, we repeated this type of experiment with a mutant nAChR that deactivates more slowly (εT12′P; Ohno et al., 1995); in this case, the ratio was estimated to be ~0.01 (Fig. 11 B). In other words, a value of ~1% seems to be a more accurate estimate of the ratio of the current carried by TMA⁺ through the nAChR relative to the current carried by the mixture of K⁺, Na⁺, Ca²⁺, and Mg²⁺. In the case of GLIC, the response was very similar to that of the nAChR; we found the corresponding ratio to be ~0.02 (Fig. 11 C), although, owing to the fast deactivation time course of GLIC (time constant = 0.91 ± 0.20 ms, in the absence of TMA⁺; n = 11), this number is likely to be an upper bound. Figure 11 D summarizes the numerical values obtained from these experiments.

In striking contrast, the ratio of intra–pulse-to-tail current values corresponding to ELIC was much larger than those obtained for the nAChR or GLIC. Indeed, this ratio was ~0.25 for wild-type ELIC and ~0.35 for the wider-pore mutant (Fig. 12, A–C). We also measured the amplitude of inward single-channel currents elicited by 10 mM cysteamine at ~80 mV in outside-out patches bathed by either the K⁺-Na⁺-Ca²⁺-Mg²⁺ solution or the 142-mM TMA⁺ solution on the extracellular side (Fig. 12 D). Under these conditions, we found the ratio of unitary-current amplitudes of wild-type ELIC to be 0.22 ± 0.01 (n = 13), a value that is very similar to that estimated from macroscopic current recordings (Fig. 12, A–C). Similar attempts to record single-channel currents carried by TMA⁺ alone through the nAChR or GLIC proved unsuccessful, which is hardly surprising given the small amplitude of the macroscopic currents shown in Fig. 11.

We also tested whether TEA⁺ permeates through the pore of ELIC. Using the same type of pulse protocol as that illustrated for TMA⁺ in Fig. 12 (A and B), we found the ratio between the current value reached at the end of the pulse of TEA⁺ plus agonist and the peak value reached upon switching the external solution to the mixture of K⁺, Na⁺, Ca²⁺, and Mg²⁺ to be ~0.09 (Fig. 12 E). That is, with a solution containing (in mM) 142 TEACl, 10 cysteamine chloride, and 10 HEPES/TEAOH, pH 7.4 on the extracellular side, the inward currents were as large as ~9% of their value when the extracellular solution consisted of (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl₂, 1.7 MgCl₂, and 10 HEPES/KOH, pH 7.4. Nearly the same value (~0.10) was obtained with the L9′A + F16′L double mutant of ELIC (Fig. 12, F and G), indicating that the larger side chains of leucine at position 9′ and phenylalanine at position 16′ do not affect the rate of TEA⁺ permeation through the channel. Collectively, the results with TMA⁺ and TEA⁺ strongly suggest that, in the open-channel conformation, the pore of ELIC is wider at its narrowest constriction than are the pores of the muscle nAChR or GLIC.

Although TMA⁺ and TEA⁺ permeate faster through ELIC than they do through the nAChR or GLIC, as previously mentioned, the currents these cations carry through ELIC when present as the only extracellular...
cations are nevertheless smaller than the current carried by the mixture of K⁺, Na⁺, Ca²⁺, and Mg²⁺ (by a factor of ~3–4 in the case of TMA¹ and ~11 in the case of TEA¹). However, the addition of TMA¹ or TEA¹ (up to a concentration of 50 mM) to the K⁺-Na⁺-Ca²⁺-Mg²⁺ solution had hardly any effect on the size of the peak-current amplitudes carried by this mixture of inorganic cations alone (Figs. 5 and 9). Thus, this lack of blockade by TMA¹ or TEA¹ cannot be ascribed to the channel being too narrow to enter the pore (because these cations certainly conduct currents) or to TMA¹ and TEA¹ permeating as fast as the mixture of inorganic cations (because the currents carried by TMA¹ and TEA¹ are smaller). Thus, it seems as though the only explanation for the lack of current block illustrated in Figs. 5 and 9 is that TMA¹ and TEA¹ interact with the open-channel pore of ELIC with such low affinity that the other cations also present in the extracellular solution—that is, K⁺ (142 mM), Na⁺ (5.4 mM), Ca²⁺ (1.8 mM), and Mg²⁺ (1.7 mM)—outcompete them, at least when TMA¹ and TEA¹ are present at a concentration of 50 mM. To test this idea, we repeated the competition experiments now using a higher concentration of TEA¹ and a simpler background solution (Fig. 13). More specifically, the TEA¹-containing solution consisted of (in mM): 142 KCl, 142 TEACl, 10 cysteamine chloride, and 10 HEPES/KOH, pH 7.4; the solution flowing through the other barrel of the theta tube (that is, the TEA¹-free solution) consisted of (in mM): 142 KCl and 10 HEPES/KOH, pH 7.4.

Under these conditions, we found that the current carried by the equimolar TEA¹-K⁺ solution was ~53% of that recorded upon TEA¹ removal, i.e., in the presence of 142 mM K⁺ alone, in the case of the wild type, and ~54% in the case of the wider-pore mutant (Fig. 13 C). Evidently, a higher concentration of TEA¹ is required to block K⁺ currents through ELIC than is required in the case of the nAChR or GLIC. Finally, we reasoned that—when present at the same concentration—a quaternary-ammonium cation larger than TEA¹ would block K⁺ currents to a larger extent. As shown in Fig. 14, this expectation was fully borne out by experiments with 142 mM tetrapropylammonium (TPA¹) chloride (TPACl; Fig. 14 A); in the presence of an equimolar mixture of KCl and TPACl (both at a concentration of 142 mM) applied to the extracellular side of ELIC, the current was ~30% as large as that carried by the K⁺ solution alone. Fig. 14 also shows that 142 mM TPA¹ carries a small but measurable current through ELIC when present as the only cation on the extracellular side (amounting to ~3.5% of the current carried by the mixture of K⁺, Na⁺, Ca²⁺, and Mg²⁺ alone; Fig. 14 B), which is intriguing in light of the large diameter of this cation (~7.8 Å; Conway et al., 1966; Edward, 1970; Ue, 1994).

It may be argued that the cation-conduction properties of ELIC could have been characterized much more directly and in more quantitative detail at the single-channel
nearly impossible to achieve using single-channel recordings. Thus, we felt that it was desirable to consider an experimental design that could be applied to all three channels under the same experimental conditions. The importance of including a second bacterial channel in the comparison seemed to fully justify the more indirect nature of macroscopic recordings.

**Leucine-to-alanine mutations at position 9’ speed up the deactivation of ELIC**

To gain insight into the interconversion among the closed, open, and desensitized states of ELIC, we compared the effects of reducing the hydrophobicity of the pore lining on the kinetics of deactivation. Channel deactivation is the decay of the macroscopic current that occurs on agonist removal, and thus, its kinetics depend on the rates of agonist dissociation and closed–open–desensitized state interconversions, with the contribution of each of these rates varying among different channels (Jones and Westbrook, 1995; Elenes et al., 2006). On the other hand, for channels that activate much faster than they desensitize, the kinetics of desensitization measured at saturating concentrations of agonist—that is, the kinetics of the macroscopic current decay that occurs during the application of agonist—depend on the rates at which the channel enters and leaves the desensitized state(s) while fully bound to the ligand. Thus, the time courses of deactivation and desensitization reflect different (although somewhat overlapping) sets of rates.

For these experiments, we chose the side chain at position 9’ (a leucine in all subunits of the muscle nAChR and ELIC, and an isoleucine in GLIC) because the effect of mutations at this position on the kinetics of deactivation—or, its single-molecule equivalent, the mean duration of bursts of single-channel openings (Wyllie et al., 1998)—has been extensively documented for the pLGICs from vertebrates (for example: Filatov and White, 1995; Labarca et al., 1995; Chang and Weiss, 1998; Kosolapov et al., 2000; Bianchi and Macdonald, 2001; Papke and Grosman, 2014). Fig. 15 illustrates the effect of shortening these side chains by mutation to alanine in the muscle nAChR and GLIC. The presence of a mutant alanine at this position of the two α subunits of the nAChR and in all five subunits of GLIC slowed down deactivation (by factors of ~90 and ~178, respectively; Table 4), a phenomenon shared by all other pLGICs for which the effect of this type of mutation on deactivation has been recorded. However, in ELIC, the leucine-to-alanine mutation sped up deactivation, with the time constant of the monoexponential fit being shortened by a factor of ~3.5 (Fig. 16 and Table 4; see also Gonzalez-Gutierrez et al., 2012). To rule out the possibility that the phenylalanine at the pore-lining position 16’ of ELIC has anything to do with this unexpected behavior (indeed, five phenylalanines at this
position seem to occur only in some bacterial and invertebrate homologues whose functional properties have not been extensively characterized yet), we also recorded the deactivation time course of the wider-pore L9′A + F16′L mutant that we used in our previously mentioned permeation studies; a leucine at position 16′ is present in four of the five subunits of the muscle nAChR, whereas an isoleucine at this position is present in all five subunits of GLIC. Remarkably, the deactivation time course of this double mutant of ELIC was faster too, also by a factor of ~3.5 (Fig. 16, C and F; and Table 4; Gonzalez-Gutierrez et al., 2012). Mutating the leucine at position 9′ of ELIC to glutamine or glutamate—two polar amino acids—in the wild-type background gave rise to, essentially, the same result: these mutations did not slow down the deactivation time course of ELIC (Fig. 16, D–F; and Table 4).

As for desensitization, the effect of mutating the leucine at position 9′ of ELIC to alanine (both in the wild-type and the F16′L backgrounds) was unremarkable: the decay of the macroscopic current became much slower, to the extent of being negligible during the 5-s applications of 10 mM cysteamine (Fig. 9 A), largely as observed for the muscle nAChR (Filatov and White, 1995; Papke and Grosman, 2014), GLIC (Bocquet et al., 2007; Gonzalez-Gutierrez et al., 2012), and all other pLGICs examined to date (e.g., Bianchi and Macdonald, 2001).

Collectively, the effects of mutations at position 9′ of the nAChR and GLIC on the time courses of deactivation and desensitization suggest that reducing the hydrophobicity of the transmembrane pore-lining destabilizes the closed and desensitized states of these two channels relative to the open state. (Although changes in the agonist-dissociation rate constant would have contributed to affect the kinetics of deactivation, we deem it unlikely for a mutation in the middle of the M2 α-helix to affect the unbinding kinetics from the distant transmitter-binding sites.) This proposed relative stabilization of the open state is consistent with the longer clusters of single-channel openings and the higher closed-to-open gating equilibrium constant of nAChR 9′ mutants inferred from unitary currents recorded at saturating concentrations of agonist (Cymes et al., 2002). In marked contrast, the same experimental maneuvers applied to ELIC destabilize the open and the desensitized states, with the destabilization of the latter being larger. That the open state of ELIC becomes
A more polar lining increases the affinity of ELIC’s pore for cysteamine

The responses of the glutamine and glutamate mutants of ELIC to cysteamine pulses (Fig. 16, D and E) differed from those recorded from the other tested constructs (Fig. 16, A–C) in that the currents transiently rose upon cysteamine removal. The solutions alternately bathing the outside-out patches in these experiments were the K+-Na+-Ca2+-Mg2+ solution with or without 10 mM cysteamine, and thus, the observed current overshoots indicate that this agonist blocked the currents carried by these two mutants to some extent (with $pK_{a1}$ and $pK_{a2}$ values of $\sim 8.3$ and $\sim 10.8$ [Avdeef and Brown, 1984], a 10-mM cysteamine solution at pH 7.4 is expected to contain $\sim 8.9$ mM of the doubly protonated, positively charged form). However, a careful examination of the electrophysiological responses recorded from the wild

destabilized relative to the closed state upon mutation was also evident at the single-channel level, in recordings performed at saturating concentrations of cysteamine that showed an intracluster open probability lower than the wild-type’s (Gonzalez-Gutierrez et al., 2012).

Admittedly, we have not tested the effect of all other natural side chains at position 9’ of ELIC, but the results obtained with alanine, glutamine, and glutamate seem compelling enough to conclude that, in this channel, the relationship between pore hydrophobicity, pore-water content, and the relative stabilities of the closed, open, and desensitized states is quite unique. To our knowledge, ELIC is the only pLGIC studied to date that deviates from the rule that mutations that reduce the hydrophobicity of the transmembrane pore lining stabilize the open-channel conformation relative to both the closed and desensitized states.

A more polar lining increases the affinity of ELIC’s pore for cysteamine

The responses of the glutamine and glutamate mutants of ELIC to cysteamine pulses (Fig. 16, D and E) differed from those recorded from the other tested constructs (Fig. 16, A–C) in that the currents transiently rose upon cysteamine removal. The solutions alternately bathing the outside-out patches in these experiments were the K’-Na’-Ca2’-Mg2’ solution with or without 10 mM cysteamine, and thus, the observed current overshoots indicate that this agonist blocked the currents carried by these two mutants to some extent (with $pK_{a1}$ and $pK_{a2}$ values of $\sim 8.3$ and $\sim 10.8$ [Avdeef and Brown, 1984], a 10-mM cysteamine solution at pH 7.4 is expected to contain $\sim 8.9$ mM of the doubly protonated, positively charged form). However, a careful examination of the electrophysiological responses recorded from the wild
The atypical conduction and gating properties of ELIC

DISCUSSION

Before this work, the characterization of two bacterial pLGICs had suggested that the functional properties of the noneukaryotic members of the superfamily fell well within the range of variability revealed by decades of

Figure 13. TEA⁺–K⁺ competition in ELIC. (A and B) Macroscopic current responses to 500-ms pulses of 10 mM cysteamine plus 142 mM TEA⁺ recorded at ~80 mV from the wild type (A) and the L9’A + F16’L wider-pore mutant (B) in the outside-out configuration. The TEA⁺-containing solution was (in mM) 142 KCl, 142 TEACL, 10 cysteamine, and 10 HEPES/KOH, pH 7.4, whereas the TEA⁺-free solution was (in mM) 142 KCl and 10 HEPES/KOH, pH 7.4. In the schematic representations of the theta-tubing perfusion, arrows indicate the application of TEA⁺. (C) Intra-pulse-to-tail current ratios. The plotted values are means obtained from 9 (wild type) and 3 (L9’A + F16’L mutant) patches; error bars are the corresponding standard errors. Both current traces shown in this figure are the averages of 10 consecutive responses recorded from two representative patches.

Figure 14. TPA⁺–K⁺ competition and TPA⁺ conduction through ELIC. (A and B) Macroscopic current responses to 500-ms pulses of 10 mM cysteamine plus 142 mM TPA⁺ recorded at ~80 mV from the wild type in the outside-out configuration. In (A), the TPA⁺-containing solution was (in mM) 142 KCl, 142 TPACL, 10 cysteamine, and 10 HEPES/KOH, pH 7.4, whereas the TPA⁺-free solution was (in mM) 142 KCl and 10 HEPES/KOH, pH 7.4. In (B), the TPA⁺-containing solution was (in mM) 142 TPACL, 10 cysteamine, and 10 HEPES/TPAOH, pH 7.4, whereas the TPA⁺-free solution was (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl₂, 1.7 MgCl₂, and 10 HEPES/KOH, pH 7.4. In the schematic representations of the theta-tubing perfusion, arrows indicate the application of TPA⁺. (C) Intra-pulse-to-tail current ratios. The plotted values are means obtained from 5 patches for each condition; error bars are the corresponding standard errors. Both current traces shown in this figure are the averages of 10 consecutive responses recorded from two representative patches.
work on their animal—both vertebrate and invertebrate—counterparts. Indeed, the differences identified between the bacterial and animal pLGICs were not much larger than those found between distantly related pLGICs from animals. For example, although the notion that GLIC is gated by an unusual agonist may have seemed surprising, it was already known that roundworms, mites, flies, and polychaete worms also have proton-gated pLGICs (Schnizler et al., 2005; Mounsey et al., 2007; Beg et al., 2008; Juneja et al., 2014), and that humans, dogs and cows have Zn2+-gated pLGICs (Davies et al., 2003; Houtani et al., 2005). Also, although the slow activation of ELIC upon fast exposure to a saturating concentration of a high-efficacy agonist (time constant ≈ 7.3 ms in outside-out patches excised from HEK-293 cells; Mott et al., 2001). Moreover, although the presence of a ring of five pore-occluding phenylalanines may have seemed a unique property of ELIC, examination of invertebrate genomes had revealed the existence of several pLGIC subunits from roundworms, sea squirts, and sea anemones that also contain a phenylalanine at position 16’ of the transmembrane M2 α-helix and that may also assemble as homopentamers in vivo (Beg and Jorgensen, 2003; Satoh et al., 2006; Putnam et al., 2007; Rufener et al., 2009). Furthermore, nothing seemed particularly remarkable about the single-channel conductance values of GLIC and ELIC. Indeed, GLIC’s value (~8 pS; Bocquet et al., 2007) is similar to that of the 5-HT3AR–5-HT3BR heteromer (~16 pS; Davies et al., 1999), whereas ELIC’s (~84 pS; Zimmermann and Dutzler, 2011) is nearly the same as that of the adult-muscle nAChR (~73 pS; Elenes et al.,

![Figure 15](https://example.com/figure15)

Figure 15. Effect of mutations at position 9’ of M2 on deactivation of the muscle nAChR and GLIC. (A and B) Macroscopic current responses to 1-ms pulses of 100-µM ACh recorded at ~80 mV from the wild-type mouse muscle adult-type nAChR (A) and the αL9’A mutant (B) in the outside-out configuration. The solutions flowing through the two barrels of the perfusion tubing were (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl2, 1.7 MgCl2, and the pH was buffered with 10 HEPES/KOH (pH 7.4), 10 TAPS/KOH (pH 9.0) or 10 acetic-acid/KOH (pH 4.5). In the case of the gain-of-function I9’A mutant, the (proton-gated) activity of the channel at pH 7.4 was relatively high, and hence, the pH of the solution applied during the “no-agonist” intervals was increased to 9.0. For all panels, the insets emphasize the time courses of deactivation; lines are fits to monoeXponential-decay functions. (E) Mutant-construct deactivation time constants obtained from monoeXponential fits normalized to the corresponding wild-type time constants. The plotted values are means obtained from 4 (L9’A nAChR) and 2 (I9’A GLIC) patches. An error bar (standard error) is only displayed for the nAChR; for GLIC, the two averaged values were 155 ms and 169 ms. All current traces shown in this figure are the averages of 10–25 consecutive responses recorded from representative patches.
2009) for inward currents recorded under comparable ion conditions.

In contrast, here, we presented experimental evidence for the notion that the superfamily of nicotinic receptor-like channels is functionally more diverse than previously thought. We found that ELIC displays a remarkably atypical response to several perturbations that have long been used to probe the pLGICs from animals. Specifically, ELIC is not blocked by quaternary-ammonium cations TMA+ or TEA+ applied extracellularly at a concentration as high as 50 mM; displays a slower macroscopic current-decay time course in the presence of lidocaine and a saturating concentration of agonist; binds lidocaine in the cavities delimited by the M1, M2, and M3 transmembrane α-helices; and deactivates with wild-type-like kinetics—or even faster—upon the introduction of mutations that reduce the hydrophobicity of the channel’s transmembrane pore lining. Instead, all other cation-selective pLGICs studied to date are blocked by quaternary-ammonium cations TMA+ or TEA+ applied extracellularly at a concentration as high as 50 mM; displays a slower macroscopic current-decay time course in the presence of a saturating concentration of agonist; binds a concentration of agonist that elicits only a half-maximal response (EC₅₀). In contrast, in our experiments, ELIC currents were elicited by a saturating concentration of cysteamine. Thus, we surmise that the reported inhibitory effect of TMA+ and TEA+ reflects the competition of these quaternary-ammonium cations (which, when applied alone, do not elicit any measurable current response; Thompson et al. [2012]) with GABA for the channel’s agonist-binding sites rather than the blocking of the pore. Indeed, it has been reported that TMA+ competes with cysteamine (Zimmermann et al., 2012) for the agonist-binding sites of ELIC, but their relative affinities are such that, at a concentration of cysteamine as high as 10 mM (i.e., the value we used in our experiments), TMA+ is expected to be outcompeted even when present at a concentration of 50 mM. Therefore, there is no discrepancy between our results and those reported by Thompson et al. (2012).

<table>
<thead>
<tr>
<th>Channel</th>
<th>τₑ (mean ± SE; ms)</th>
<th>τₑ (range; ms)</th>
<th>P-value</th>
<th>Number of patches</th>
</tr>
</thead>
<tbody>
<tr>
<td>Wild-type nAChR</td>
<td>1.12 ± 0.10</td>
<td>0.77–1.71</td>
<td>1.0 × 10⁻¹⁵</td>
<td>12</td>
</tr>
<tr>
<td>αL9 ‘A AChR</td>
<td>100 ± 5</td>
<td>88.9–112</td>
<td>–</td>
<td>4</td>
</tr>
<tr>
<td>Wild-type GLIC</td>
<td>0.91 ± 0.20</td>
<td>0.41–1.91</td>
<td>–</td>
<td>11</td>
</tr>
<tr>
<td>19 ‘A GLIC⁺</td>
<td>162</td>
<td>155; 169</td>
<td>–</td>
<td>2</td>
</tr>
<tr>
<td>Wild-type ELIC</td>
<td>17.2 ± 3.2</td>
<td>7.34–26.3</td>
<td>–</td>
<td>6</td>
</tr>
<tr>
<td>L9 ‘A ELIC</td>
<td>5.01 ± 0.95</td>
<td>4.02–9.23</td>
<td>2.7 × 10⁻⁵</td>
<td>6</td>
</tr>
<tr>
<td>L9 ‘A + F16 ‘L ELIC</td>
<td>5.11 ± 1.04</td>
<td>4.01–9.61</td>
<td>3.0 × 10⁻⁵</td>
<td>6</td>
</tr>
<tr>
<td>L9 ‘Q ELIC</td>
<td>15.3 ± 1.9</td>
<td>8.75–18.4</td>
<td>0.60</td>
<td>6</td>
</tr>
<tr>
<td>L9 ‘E ELIC</td>
<td>12.6 ± 0.9</td>
<td>10.4–15.3</td>
<td>0.17</td>
<td>6</td>
</tr>
</tbody>
</table>

*High-quality recordings could only be obtained from two outside-out patches. Hence, neither the standard error nor the p-value was calculated.

No discrete feature of the amino-acid sequence of ELIC seemed “suspicious” to us so as to anticipate its unique pore properties, and thus, it seems impossible to predict ELIC-like behavior in newly discovered pLGIC subunits on the basis of sequence gazing alone. Furthermore, because only a structural model for a nonconductive crystallized conformation of ELIC is currently available (Hilf and Dutzler, 2008), identifying the three-dimensional structural basis for its unusual open-channel behavior does not seem straightforward, either. Perhaps, however, the lack of block by 50 mM TMA+ or TEA+ would be the simplest property to explain if the most intracellular turn of each of the five M2 α-helices moved little upon opening (relative to their position in the nonconductive crystallized conformation) and formed the narrowest constriction in the open-channel conformation. Indeed, the diameter of the pore at the level of the intracellular ends of the M2 α-helices in the crystallized...
nonconductive conformation of ELIC is 9 Å, a size that would be consistent with the relatively high permeation rate observed for TMA⁺, TEA⁺, and TPA⁺. For comparison, in a homology model of the open-channel conformation of the mouse muscle nAChR, this diameter is 7 Å (Harpole and Grosman, 2014), whereas in the open-channel model of GLIC (Protein Data Bank ID code 4HFI; Sauguet et al., 2013), it is 5.2 Å (forcing the side chains of the five pore-lining glutamates at position –2 to move out of the way by adopting a rotamer with $\chi_1 \approx -60^\circ$ and $\chi_2 \approx +60^\circ$; otherwise, the diameter would be even narrower). It is tempting to speculate that it is this putatively larger size of the transmembrane pore cavity in the open state of ELIC that also underlies the lower binding affinity for TMA⁺ and TEA⁺, and the atypical effect of mutations to pore-lining residues on the kinetics of deactivation.

The physiological role of ELIC in the bacterium Erwinia chrysanthemi (now reclassified as Dickeya dadantii) is not known. However, we reason that the low affinity of ELIC for quaternary-ammonium cations, for example, would be advantageous if the channel faced an external solution that is rich in hydrophobic cations, and yet, the bacterium required a fast influx of inorganic cations—such as Na⁺ and Ca²⁺—through the channel’s cation-selective pore. In addition, it is likely that permeant organic cations for which the pore of ELIC has a higher affinity (higher than for TMA⁺, TEA⁺ or TPA⁺) exist. If this were the case, and if such cations indeed existed in the solutions bathing the bacterial membrane, then ELIC could function as a channel for solutes other than small inorganic cations. Clearly, extensive future work will be required to elucidate how the peculiar properties of this channel give rise to its biological function. Moreover, there may well be other pLGICs that behave like ELIC among the largely unexplored bacterial, archaeal, and invertebrate members of the superfamily, and thus, ELIC’s unconventional features may turn out to be less unusual than we currently think.

As for its role as a model system for the entire superfamily, our data indicate that caution should be exercised when generalizing results obtained with ELIC to the rest of the pLGICs, especially as they pertain to the properties of the transmembrane pore domain. Nevertheless, we would like to emphasize the notion that a member with such different functional properties in the context of a well-conserved three-dimensional architecture offers an unparalleled opportunity to further

![Figure 16. Effect of mutations at position 9' of M2 on deactivation of ELIC. (A–E) Macroscopic current responses to 500-ms pulses of 10 mM cysteamine recorded at –80 mV from wild-type ELIC and the indicated mutants in the outside-out configuration. The solutions flowing through the two barrels of the perfusion tubing were (in mM) 142 KCl, 5.4 NaCl, 1.8 CaCl₂, 1.7 MgCl₂, and 10 HEPES/KOH, pH 7.4 with or without cysteamine. The insets emphasize the time courses of deactivation; lines are fits to monoexponential-decay functions. (F) Mutant-construct deactivation time constants obtained from monoexponential fits normalized to the wild-type time constant. The plotted values are means obtained from 6 patches for each mutant; error bars are the corresponding standard errors. All current traces shown in this figure are the averages of 10 consecutive responses recorded from representative patches.](image-url)
our mechanistic understanding of the pLGICs from vertebrate animals.

We thank Keith Brister, Joseph Brunzelle, David Smith, Elena Kondrashkina, Spencer Anderson, and Zdzislaw Wawerzk (Life Sciences Collaborative Access Team, 21 ID-D/F/G at Argonne National Laboratory, Advanced Photon Source) for technical assistance during crystallographic data collection; S. Sine (Mayo Clinic, Rochester, MN) for wild-type muscle nAChR subunit cDNAs; Y. Bello, C. Johnson, N. Kowalczyk, M. Rigby, and G. Wang for assistance with mutagenesis, cell culturing and transfections; and T. Harpole for the critical reading of the manuscript.

This work was supported by National Institutes of Health Grant NS402169 (to C. Grosman) and the Richard and Margaret Romano Professorial Scholarship (to C. Grosman).

The authors declare no competing financial interests.

Sharona E. Gordon served as editor.

Submitted: 25 November 2014
Accepted: 14 May 2015

REFERENCES


Adler, M., A.C. Oliveira, E.X. Albuquerque, N.A. Mansour, and 34 The atypical conduction and gating properties of ELIC


Grosman, C. 2003. Free-energy landscapes of ion-channel gating are malleable: changes in the number of bound ligands are accompanied by changes in the location of the transition state in acetylcholine-receptor channels. Biochemistry. 42:14977–14987. http://dx.doi.org/10.1021/bi0334334


Purohit, P., and A. Auerbach. 2013. Loop C and the mechanism of acetylcholine receptor-channel gating. J. Gen. Physiol. 141:467–478.


Gonzalez-Gutierrez and Grosman 35