Intracellular pH-regulating Mechanism of the Squid Axon

Relation Between the External Na\(^+\) and HCO\(_3^-\) Dependences

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ABSTRACT The intracellular pH-regulating mechanism of the squid axon was examined for its dependence on the concentrations of external Na\(^+\) and HCO\(_3^-\), always at an external pH (pH\(_e\)) of 8.0. Axons having an initial intracellular pH (pH\(_i\)) of ~7.4 were internally dialyzed with a solution of pH 6.5 that contained 400 mM Cl\(^-\) and no Na\(^+\). After pH\(_i\) had fallen to ~6.6, dialysis was halted, thereby returning control of pH\(_i\) to the axon. With external Na\(^+\) and HCO\(_3^-\) present, intracellular pH (pH\(_i\)) increased because of the activity of the pH\(_i\)-regulating system. The acid extrusion rate (i.e., equivalent efflux of H\(^+\), J\(_H\)) is the product of the pH\(_i\) recovery rate, intracellular buffering power, and the volume-to-surface ratio. The [HCO\(_3^-\)]\(_e\) dependence of J\(_H\) was examined at three fixed levels of [Na\(^+\)]\(_e\): 425, 212, and 106 mM. In all three cases, the apparent J\(_{max}\) was ~19 pmol·cm\(^{-2}\)·s\(^{-1}\). However, the apparent K\(_m\) (HCO\(_3^-\)) was approximately inversely proportional to [Na\(^+\)]\(_e\), rising from 2.6 to 5.4 to 9.7 mM as [Na\(^+\)]\(_e\) was lowered from 425 to 212 to 106 mM, respectively. The [Na\(^+\)]\(_e\) dependence of J\(_H\) was similarly examined at three fixed levels of [HCO\(_3^-\)]\(_e\): 12, 6, and 3 mM. The J\(_{max}\) values did not vary significantly from those in the first series of experiments. The apparent K\(_m\) (Na\(^+\)), however, was approximately inversely related to [HCO\(_3^-\)]\(_e\), rising from 71 to 174 to 261 mM as [HCO\(_3^-\)]\(_e\) was lowered from 12 to 6 to 3 mM, respectively. These results agree with the predictions of the ion-pair model of acid extrusion, which has external Na\(^+\) and CO\(_3^-\) combining to form the ion pair NaCO\(_3^-\), which then exchanges for internal Cl\(^-\). When the J\(_H\) data are replotted as a function of [NaCO\(_3^-\)]\(_e\), data from all six groups of experiments fall along the same Michaelis-Menten curve, with an apparent K\(_m\) (NaCO\(_3^-\)) of 80 \(\mu\)M. The ordered and random binding of Na\(^+\) and CO\(_3^-\) cannot be ruled out as possible models, but are restricted in allowable combinations of rate constants.
INTRODUCTION

The intracellular pH (pHi) of the squid giant axon is regulated by a mechanism, located in the cell membrane, that mediates the uptake of both Na⁺ and HCO₃⁻ (or a related ion) and the efflux of Cl⁻ and possibly H⁺. This mechanism responds to decreases in pHi by increasing its rate of transport (i.e., acid extrusion). Its stoichiometry is one mole of Na⁺ taken up for each mole of Cl⁻ lost and for every two equivalents of acid neutralized inside the cell (Boron and Russell, 1983). Fig. 1 illustrates four models that can account for this stoichiometry. The first (Fig. 1A) has Na⁺ and HCO₃⁻ exchanging for Cl⁻ plus H⁺ (Thomas, 1977). In the second (Fig. 1B), the exit of H⁺ is replaced by the entry of a second HCO₃⁻. In the third model (Fig. 1C), the entry of two HCO₃⁻ is replaced by that of a single CO₃²⁻. Finally, in the fourth model (Fig. 1D), the separate entry of Na⁺ and CO₃²⁻ is replaced by the entry of a single NaCO₃ ion pair (Becker and Duhm, 1978). Although these four models are equivalent thermodynamically, they do not necessarily lead to identical kinetic predictions. In particular, the ion-pair model requires that the acid extrusion rate (j_H⁺) be a unique function of neither
extracellular [Na⁺] ([Na⁺]₀) or [HCO₃⁻], but rather of [NaCO₃]₀. At a fixed pH₀,
[NaCO₃]₀ is proportional to the product [Na⁺]₀.[HCO₃⁻].

pH-regulating mechanisms qualitatively similar to the squid axon's have been
described in snail neurons (Thomas, 1977), crayfish neurons (Moody, 1981), and
barnacle muscle (Boron et al., 1981). In particular, the transporters in all four
preparations are blocked by 4-acetamido-4'-isothiocyano-2,2'-disulfonate (SITS),
and involve internal Cl⁻ as well as external Na⁺ and HCO₃⁻. Kinetic analyses are
limited to the squid axon (Boron and Russell, 1983) and barnacle muscle (Boron
et al., 1981). In both preparations, Michaelis-Menten kinetics adequately describe
the dependence of Jₜ on [Na⁺]₀ at a single [HCO₃⁻]₀ (12 and 10 mM, respectively,
for squid and barnacle), as well as the dependence of Jₜ on [HCO₃⁻]₀ at a single
[Na⁺]₀ (425 and 440 mM). The ion-pair model requires that plotting these Jₜ
data as a function of the calculated [NaCO₃]₀ should cause all the data to fall
along the same Jₜ vs. [NaCO₃]₀ curve, regardless of whether [Na⁺]₀ was varied
at a single [HCO₃⁻]₀ or vice versa. The aforementioned data fulfill this prediction
for both squid axons and barnacle muscle. However, when the barnacle study
was extended to include the dependence of Jₜ on [Na⁺]₀ at a second fixed level
of [HCO₃⁻]₀ (i.e., 2.5 mM), the additional data fell on a Jₜ vs. [NaCO₃]₀ curve
very different from the first. Thus, taken together, the Jₜ vs. [Na⁺]₀ data at 2.5
and 10 mM HCO₃⁻ allow us to rule out the ion-pair model for barnacle muscle.
The question that arises is whether a more extensive kinetic analysis on the squid
axon would produce data that are also inconsistent with the ion-pair model.
Given several other minor differences between the pH-regulating systems of
barnacle muscle and squid axons (see Discussion), I felt the likelihood of substan-
tial kinetic discrepancies to be significant.

In the present work, I examine Jₜ as a function of [Na⁺]₀ at three fixed levels
of [HCO₃⁻]₀, and as a function of [HCO₃⁻]₀ at three fixed levels of [Na⁺]₀. The
present study is more complete than the earlier one on barnacle (Boron et al.,
1981), in which Na⁺ dependence was examined at only two [HCO₃⁻]₀ values and
HCO₃⁻ dependence was examined at only one [Na⁺]₀. Furthermore, whereas the
previous kinetic studies on either barnacle or squid were performed on intact
cells, the present study was performed on internally dialyzed axons. This per-
mitted tight control of the intracellular environment with respect to Na⁺ and
Cl⁻, and thus it had two theoretical advantages over the earlier kinetic studies:
(a) because the dialysate was Na⁺ free, the reverse reaction, in which Na⁺ plus
HCO₃⁻ (or an equivalent species) could leave the cell, was obviated; (b) because
[Cl⁻] was very high in the dialysate, the transporter was nearly saturated with
respect to internal Cl⁻. I found that all of the present data fall along a single Jₜ
vs. [NaCO₃]₀ curve. The results are thus consistent with the ion-pair model and
place restrictions on other kinetic models.

METHODS

General

The experiments were conducted at the Marine Biological Laboratory, Woods Hole, MA,
during May and June, 1983. Live specimens of the squid Loligo pealei were decapitated,
and the first stellar nerve from each side was removed and placed in cold Woods Hole
A 4-5-cm length of giant axon (generally 400–600 μm in diameter) was isolated from the nerve by microdissection, cannulated at both ends, and mounted horizontally in a chamber (see Boron and Russell, 1983) designed for internal dialysis (Brinley and Mullins, 1967). A length of dialysis tubing (see below) was threaded through one cannula, down the length of the axon, and out the opposite cannula. In addition, pH- and voltage-sensitive microelectrodes were introduced through opposite cannulas, so that their tips were within 500 μm of each other at the middle of the axon. Artificial seawater continuously flowed around the axon. The temperature, controlled by a circulating water bath connected to the water jacket on the underside of the chamber, was 22°C.

**Solutions**

The standard external fluid (i.e., squid seawater [SSW]) had the following composition (in mM): 425.2 Na⁺, 12 K⁺, 3 Ca²⁺, 57.5 Mg²⁺, 531 Cl⁻, 12 HCO₃⁻, 0.1 EDTA⁻, 15 of the anionic form of [2-hydroxyethyl]-1-piperazine-propane sulfonic acid (EPPS), and 15 of the neutral form of EPPS (pKₐ ~ 8.0). The pH was 8.00, and the osmolality was ~980 mosmol. In experiments in which [Na⁺] was lowered, the Na⁺ was replaced mole for mole by N-methyl-D-glucammonium, the latter made by titrating the free base (Sigma Chemical Co., St. Louis, MO) with HCl. When [HCO₃⁻] was varied, HCO₃⁻ was exchanged for Cl⁻ on a mole-for-mole basis.

The HCO₃⁻-containing seawaters were made as follows. All components except HCO₃⁻ (added as the K⁺ or Na⁺ salt) were combined and brought to 99% of the final volume, and then titrated to pH 8.00 with HCl or N-methyl-D-glucamine. For solutions having an [HCO₃⁻] of ≤12 mM, KHCO₃ was then added from a 1.21 M stock solution. HCO₃⁻-containing SSWs having a [HCO₃⁻] of 24 or 48 mM were made similarly, except that the HCO₃⁻ was added as powdered NaHCO₃. The addition of HCO₃⁻ caused the pH to decrease anomalously (by ~0.03 in the case of 12 mM HCO₃⁻), probably because more of the added HCO₃⁻ underwent the reaction HCO₃⁻ → H⁺ + CO₂ than underwent the alternative reaction sequence HCO₃⁻ + H⁺ → H₂CO₃ → H₂O + CO₂. The pH was returned to 8.00 by briefly gassing the solution with 100% O₂ while vigorously stirring. Inasmuch as the CO₂ evolution procedure required a few minutes, there is little doubt that the CO₂ dehydration reaction (time constant at room temperature, ~0.04 s) was allowed sufficient time to go to completion. Because ~1% of the added HCO₃⁻ goes on to form CO₂ and another ~1% goes on to form CO₃⁻, the actual [HCO₃⁻] is at least ~2% lower than the nominal value. In addition, the CO₂ evolution procedure for returning the pH to 8.00 probably causes the loss of another ~4% of HCO₃⁻ at a nominal [HCO₃⁻] of 48 mM, ~2.5% at a nominal [HCO₃⁻] of 12 mM, and correspondingly smaller losses at lower nominal HCO₃⁻ concentrations. The SSW was drawn up into 140-ml plastic syringes, which were then capped. Such solutions can be stored in the refrigerator for at least 18 h and still maintain the proper pH and (by bioassay) pCO₂. The advantage of making HCO₃⁻-containing solutions in this way is that the technique obviates the need for expensive gas mixtures. HCO₃⁻-containing SSWs were delivered to the chamber via CO₂-impermeable Saran tubing (Clarkson Equipment and Controls, Detroit, MI).

In the initial and final phases of each experiment, the axons were exposed to HCO₃⁻-free SSW. This was the same as standard SSW except that it contained only 10 mM K⁺, was HCO₃⁻-free (Cl⁻ replacing HCO₃⁻), and for purposes of economy contained only 10 mM total EPPS (MgCl₂ replacing MgEPPS on an osmole-for-osmole basis).

The internal dialysis fluid (DF) had the following composition (in mM): 0 Na⁺, 415.3 K⁺, 7 Mg²⁺, 8 Tris, 400 Cl⁻, 14 glutamate, 4 ATP⁺, 1 EGTA⁺, 15.3 of the anionic form of 2-[N-morpholino]ethanesulfonic acid (MES), 6.7 of the neutral form of MES, 215 glycine, and 0.5 phenol red. The pH was adjusted to 6.50 with HCl or KOH, and the
osmolality was adjusted to ~980 mosmol with glycine. The ATP was added to the DF on the day of the experiment from a 400-mM (pH 7.0) stock solution stored at −5°C.

Internal Dialysis

The internal dialysis technique (Brinley and Mullins, 1967) permits control of the intracellular ionic environment. Details of my use of the method can be found in an earlier paper (Boron and Russell, 1983). The dialysis capillaries (140 μm o.d.) were made of cellulose acetate tubing (Fisher Research Laboratories, FRL, Inc., Dedham, MA), an 18-mm-long portion of which was rendered porous to low-molecular-weight solutes by soaking it in 0.1 N NaOH for 18–24 h. The central region of the axon, which was dialyzed and in which the tips of the pH- and voltage-sensitive electrodes resided, was isolated from the cannulated ends of the axon by grease seals (a mixture of vaseline and mineral oil). The dialysis capillary was perfused with DF at the rate of ~5 μl/min.

Measurement of pH

As noted above, pH- and voltage-sensitive electrodes were introduced through opposite cannulas, alongside the dialysis capillary. The pH-sensitive electrodes were of the design of Hinke (1967), fabricated of lead glass (0120, Corning Glass Works, Corning, NY) and pH-sensitive glass (Clark Electromedical Instruments, Pangbourne, England). The lead glass shank had an outer diameter of <125 μm for at least the terminal 5 cm. The pH-sensitive tips had outer diameters of ~50 μm at the glass-glass seal and exposed lengths of 200–300 μm. The electrodes were filled with 0.1 M HCl and fitted with Ag/AgCl half-cells. They were calibrated in high-ionic-strength buffers (Boron and De Weer, 1976). The voltage-sensitive electrodes were similar to the pH electrodes, but had open tips (~10 μm diam), were filled with 0.5 M KCl, and were fitted with a calomel half-cell. A second calomel half-cell, the tip of which was placed directly in the SSW exit port, served as the external reference electrode. The system was grounded via a platinum/iridium wire placed in the chamber. The signals from the pH- and voltage-sensitive electrodes were amplified by separate channels of a high-impedance (10^15 Ω) electrometer (model 223, W-P Instruments, Inc., New Haven, CT), and the signal from the external reference electrode was amplified by one channel of an electrode amplifier (10^11 Ω input impedance, model M750, W-P Instruments, Inc.). The electronically obtained difference between the signals from the pH- and voltage-sensitive electrodes is the voltage due solely to pH, and was plotted by a strip-chart recorder and sampled every 10 s by an analog-to-digital converter (AD-212, Tekmar Co., Cincinnati, OH) interfaced to a Horizon computer (Northstar, San Leandro, CA). The difference between the signals from the voltage-sensitive and external reference electrodes represents membrane potential (V_m) and was processed similarly.

Calculation of Acid Extrusion Rates

I define the acid extrusion rate (f_H) as the flux (if any) of H⁺ out of the cell plus the flux of HCO₃⁻ (or a related species) into the cell. My approach was to acid load axons by dialyzing with a pH 6.5 solution, and to halt dialysis when pH reached ~6.6. The pH-regulating system then extrudes acid from the cell (provided Na⁺ and HCO₃⁻ are present in the external solution), causing pH to rise. f_H is the product of the rate of pH recovery (dpH/dt) from the imposed acid load, the axon's volume-to-surface ratio, and the total intracellular buffering power (β_T). dpH/dt was usually determined by a linear least-squares fit of the pH recovery data, previously acquired by the computer. However, the computer was nonfunctional for approximately the first 30% of the experiments and malfunctions in some of the others. For these experiments, dpH/dt was determined by
drawing a line through a strip-chart recording of the data. The volume-to-surface ratio is one-fourth of the axon’s diameter, assuming the axon to be a cylinder. \( \beta_T \) is the sum of the intrinsic or non-CO\(_2\)-buffering power \( \beta_i \) and the CO\(_2\)-buffering power \( \beta_{CO_2} \). In a previous study (Boron and Russell, 1983), it was found that the empirically determined \( \beta_i \) did not differ significantly from the calculated buffering power of the DF used in that study. Accordingly, I have assumed that in the present study \( \beta_i \) is 11.2 mM, the buffering power calculated for the present DF. \( \beta_{CO_2} \) was individually calculated for each segment of pH recovery. In a system in which CO\(_2\) can freely equilibrate with the environment, \( \beta_{CO_2} = (\ln 10) [HCO_3^-] \). [HCO\(_3\)^-] was calculated from pH, assuming equal CO\(_2\) tensions inside and outside the axon, taking as pH the value at the midpoint of the interval used to obtain \( dpH/dt \).

**Curve-fitting Procedures**

The acid extrusion rate data were fitted to the Michaelis-Menten equation using nonlinear least-squares methods (Scarborough, 1966). The equation is of the form \( J_H = sJ_{max}/(s + K_m) \), where \( s \) is substrate concentration, \( J_{max} \) is the apparent maximal \( J_H \), and \( K_m \) is the apparent Michaelis constant. Three types of fits were performed. For a type 1 fit, the data were fitted to the standard Michaelis-Menten equation, resulting in best-fit values for both \( K_m \) and \( J_{max} \). For a type 2 fit, the curve was forced through an arbitrary point, in addition to the origin. As described in the Results, for each axon I determined \( J_H \) in a “standard” solution having \([Na^+]_o = 425\) mM and \([HCO_3^-]_o = 12\) mM, and in three additional “test” combinations of \([Na^+]_o \) and \([HCO_3^-]_o \). To reduce scatter, I analyzed the data as the ratio \( J_H(\text{test})/J_H(\text{standard}) \), not as absolute fluxes. In the analysis of the dependence of \( J_H \) on \([Na^+]_o \) at a fixed \([HCO_3^-]_o \) of 12 mM, there were no independently determined values for the \( J_H(\text{test})/J_H(\text{standard}) \) ratio at a \([Na^+]_o \) of 425 mM, even though, by definition, this ratio must be unity. A similar situation existed for the analysis of the dependence of \( J_H \) on \([HCO_3^-]_o \) at a fixed \([Na^+]_o \) of 425 mM, in which case the ratio \( J_H(\text{test})/J_H(\text{standard}) \) was not determined independently at an \([HCO_3^-]_o \) of 12 mM. The following variant of the Michaelis-Menten equation forces the curve through the standard point, having coordinates \( s = s' \) and \( J_H = J' \):

\[
J = sJ'(s'+K_m)/[s'(s+K_m)].
\]

\( K_m \) is estimated from a nonlinear least-squares fit, and \( J_{max} \) is then calculated from this \( K_m \), according to the equation \( J_{max} = (s'+K_m)/s' \). A type 3 fit treats the Michaelis-Menten equation as having only one fittable parameter, \( K_m J_{max} \) is assumed to be independently known. This type of fit was used in the provisional analysis of data for which the concentration of substrate (i.e., Na\(^+\)) could not be raised sufficiently above the expected \( K_m \) to allow an optimal curve-fit determination of \( J_{max} \) and \( K_m \).

**Switching of Solutions**

The computer not only acquired the data, but also executed the solution changes. The syringe drivers that delivered the CO\(_2\)-containing SSWs (model 975, Harvard Apparatus Co., Inc., South Natick, MA) and the syringe driver that delivered the DF (model 341A, Sage Instruments Div., Cambridge, MA) were switched on and off by computer-controlled relays into which their line cords were plugged. The peristaltic pump that delivered the CO\(_2\)-free SSW (model 2132, LKB Instruments, Inc., Gaithersburg, MD) was also controlled by a computer-activated relay. The inputs and outputs of four four-way Kel-F/Teflon valves (model 201-05, Altex Scientific Inc., Berkeley, CA) were chained together, so that the valve assembly had one output to the dialysis chamber and five inputs (one from the CO\(_2\)-free SSW and four from CO\(_2\)-containing SSWs). The Altex valves were
Switched by pneumatic pistons, which in turn were activated by computer-controlled switches. Because the experimental protocol was standard, the computer could be programmed to decide when to switch solutions, based on pH, dpH/dt, and the elapsed time in a given solution.

Statistics

The $K_m$ and $J_{\text{max}}$ values, derived from nonlinear least-squares curve fits, are given ± the standard deviation. Mean values of acid extrusion rates and intracellular pH are given ± the standard error.

RESULTS

Experimental Protocol

Acid-extruding transport systems in intact cells are best studied by acutely acid loading the cell and monitoring the subsequent recovery of pH. In the present experiments, the acid loading was accomplished by dialyzing the axon with a dialysis fluid (DF) having a nominal pH of 6.5. Because the DF was also Na-free, the possible reversal of the transporter was prevented. In addition, the DF contained 400 mM Cl-. Inasmuch as a previous study (Boron and Russell, 1983) had shown that the apparent $K_m$ for internal Cl- is ~84 mM, 400 mM Cl- should have left the transporter ~83% saturated with respect to Cl-, provided the $K_m$ is not influenced by lowering [Na⁺]. A typical experiment is illustrated in Fig. 2. Initiation of dialysis (point a) causes a rapid acidification of the axoplasm. From an initial value of ~7.5, pH reaches 6.7 after ~45 min. pH probably would have approached ~6.6 had dialysis been continued for a longer period. Previous work with Na⁺ and Cl- isotopic fluxes (Boron and Russell, 1983), as well as more recent data obtained with Cl- sensitive microelectrodes (J. M. Russell, personal communication), indicate that 45 min of dialysis is sufficient for [Na⁺]i and [Cl-]i to closely approach their levels in the DF. After dialysis is halted (b), pH increases by 0.01 and then is relatively stable. This time of relative stability just before point c is the initial baseline period referred to below. When the external fluid is switched from HCO₃-free SSW to SSW containing 425 mM Na⁺ and 12 mM HCO₃ at pH 8.00, there is a slight decrease in pH (segment cd) caused by the influx of CO₂, which is followed by a rapid increase of pH (de). The pH recovery shown by segment de is due to acid extrusion by the pH-regulating system and corresponds to an acid extrusion rate ($J_H$) of 20.8 pmol·cm⁻²·s⁻¹. The subsequent reduction of [Na⁺]o to 26.5 mM at constant [HCO₃]o (ef) slows the pH recovery to a rate corresponding to a $J_H$ of 9.4 pmol·cm⁻²·s⁻¹. At point f, [HCO₃]o and pCO₂ are simultaneously reduced to one-fourth of their initial values at constant pHo (8.00) and [Na⁺]o (26.5 mM). The reduction of pCO₂ causes a rapid rise of pH, because of the efflux of CO₂ (fg), after which acid extrusion causes pH to rise at a very low rate (gh). dpH/dt in this segment corresponds to a $J_H$ of only 0.9 pmol·cm⁻²·s⁻¹. Raising [Na⁺]o to 53 mM at constant [HCO₃]o causes the pH recovery rate to increase (hi) to a level consistent with a $J_H$ of 4.1 pmol·cm⁻²·s⁻¹. Finally, when the CO₂/HCO₃ SSW is replaced by HCO₃-free SSW, there is a rapid increase of pH caused by the efflux of CO₂.
followed by a relative stabilization of $pH_i$ during the final baseline period $(jk)$.

The assumption that $J_H$ is proportional to $dpH_i/dt$ is valid only when all $pH_i$ changes are due to the $pH_i$-regulating system. However, slight drifts in the $pH_i$ baseline often occur before the $CO_2/\text{HCO}_3^-$ is introduced and/or after it is removed, and indicate that background acid or alkali loading may be influencing the calculated acid extrusion rates. Estimates of these background rates were subtracted from the gross $J_H$ values as follows. I first performed a linear fit of

![Figure 2](image-url)

**Figure 2.** Effect on acid extrusion rate of altering $[Na^+]_o$ and/or $[\text{HCO}_3^-]_o$. At point $a$, the flow of dialysis fluid (DF) was begun, leading to a gradual fall of intracellular $pH$ ($pH_i$). Because $[Na^+]_{DF} = 0$ and $[\text{Cl}^-]_{DF} = 400$ mM, the axoplasm also became low in $Na^+$ and high in $Cl^-$. At point $b$, dialysis was halted, so that the subsequent course of $pH_i$ was determined by the axon. After a slight rise, $pH_i$ stabilized at $c$ (the initial baseline), failing to recover in the absence of $\text{HCO}_3^-$. The introduction of 12 mM $\text{HCO}_3^-$ at $c$ ([Na]$^+_o = 425$ mM) caused a rapid alkalinization $(de)$. The $pH_i$ recovery was slowed by lowering [Na$^+$]$_o$ to 26.5 mM $(ef)$ while holding $[\text{HCO}_3^-]_o$ constant at 12 mM, and slowed even further by lowering $[\text{HCO}_3^-]_o$ to 3 mM while holding [Na$^+$]$_o$ constant at 26.5 mM $(gh)$. Finally, doubling [Na$^+$]$_o$ to 53 mM while holding $[\text{HCO}_3^-]_o$ constant at 3 mM increased the rate of $pH_i$ recovery $(hi)$. The rapid acidification during $cd$ was caused by the increase in $pCO_2$, whereas the rapid alkalinizations during $fg$ and $ij$ were due to decreasing $pCO_2$. $pH_o$ was 8.00 throughout.
the pH time course in the initial (the region before c) and final baseline periods (segment jk). The slopes of these lines were then converted to initial and final background acid fluxes. The background flux, which was assumed to vary linearly between the initial and final baseline periods, was then subtracted from the total calculated flux during the periods of acid extrusion (i.e., from points d through i).

Because fluxes can vary considerably from axon to axon, I normalized the data in the following manner. For each axon, a $J_H$ value was obtained under "standard" conditions of 425 mM Na$^+$/12 mM HCO$_3^-$ (e.g., de in Fig. 2) and in up to three other "test" solutions (e.g., ef, gh, and hi). Each test $J_H$ was expressed as a fraction of the standard $J_H$ for that axon. After the data analyses were complete, the ratios were converted back into fluxes by multiplying them by the mean $J_H$ in the standard solution, 15.3 ± 0.6 pmol·cm$^{-2}$·s$^{-1}$ (n = 63 axons). As expected, this standard $J_H$ is considerably higher than the value of 9.5 pmol·cm$^{-2}$·s$^{-1}$ obtained previously (Boron and Russell, 1983) on intact (i.e., undialyzed) axons, for which [Cl$^-$]$_i$ was much lower, probably on the order of 100 mM (Brinley and Mullins, 1965; Russell, 1976).

**Dependence of $J_H$ on [HCO$_3^-$]$_o$**

I determined the dependence of $J_H$ on [HCO$_3^-$]$_o$ at three fixed levels of [Na$^+$]$_o$: 425, 212, and 106 mM. The results are plotted in Fig. 3 and summarized in Table I. The $J_H$ data obtained in 425 mM Na$^+$ were fitted to a modified Michaelis-Menten equation (type 2 fit; see Methods) that forced the curve through the mean standard flux (i.e., 15.3 pmol·cm$^{-2}$·s$^{-1}$) under standard conditions (i.e., [HCO$_3^-$]$_o$ = 12 mM, [Na$^+$]$_o$ = 425 mM). This point is denoted by an asterisk in the figure. The $K_m$ (HCO$_3^-$) in 425 mM Na$^+$ was 2.6 ± 0.5 mM, which is very similar to the value of 2.3 mM previously found for intact axons (Boron and Russell, 1983). This similarity suggests that the combination of raising [Cl$^-$]$_i$ from ~100 to 400 mM and reducing [Na$^+$]$_o$ to ~0 mM has little effect on $K_m$ (HCO$_3^-$). $J_{max}$ in these experiments was 18.6 ± 2.1 pmol·cm$^{-2}$·s$^{-1}$, considerably higher than the value of 10.6 pmol·cm$^{-2}$·s$^{-1}$ obtained previously. As noted above, this discrepancy is probably due to the much higher [Cl$^-$]$_i$ in the present study. Indeed, in earlier work on dialyzed axons (Boron and Russell, 1983), in which [Cl$^-$]$_i$ was varied at a fixed [Na$^+$]$_o$ of 425 mM and a fixed [HCO$_3^-$]$_o$ of 12 mM, the $J_{max}$ was 19.6 ± 1.2 pmol·cm$^{-2}$·s$^{-1}$. This is not significantly different from the value obtained in the present study, in which [HCO$_3^-$]$_o$ was varied at high [Cl$^-$]$_i$.

The data at [Na$^+$]$_o$ values of 212 and 106 mM were fitted to an unmodified Michaelis-Menten equation (type 1 fit; see Methods). When [Na$^+$]$_o$ was reduced by half, to 212 mM, $K_m$ (HCO$_3^-$) approximately doubled, to 5.4 ± 1.0 mM. $J_{max}$, however, was 18.7 ± 1.1 pmol·cm$^{-2}$·s$^{-1}$, which is not significantly different from the value in 425 mM Na$^+$. Reducing [Na$^+$]$_o$ to one-fourth of its control value, to 106 mM, caused $K_m$ (HCO$_3^-$) to increase by a factor of >3.7, to 9.7 ± 2.1 mM. Once again, $J_{max}$ (19.2 ± 1.5 pmol·cm$^{-2}$·s$^{-1}$) was not significantly altered by the reduction of [Na$^+$]$_o$. The three $K_m$ (HCO$_3^-$) values of Table I are all significantly different from one another ($P < 0.001$).
Dependence of $J_H$ on $[Na^+]_o$

I examined the dependence of the acid extrusion rate on $[Na^+]_o$ at three different levels of $[HCO_3^-]_o$: 12, 6, and 3 mM. The results are plotted in Fig. 4 and summarized in Table II. The data at an $[HCO_3^-]_o$ of 12 mM were fitted to a modified Michaelis-Menten equation (type 1 fit), which forced the curve through the mean standard $J_H$ (i.e., 15.3 pmol·cm$^{-2}$·s$^{-1}$) under standard conditions (i.e., $[Na^+]_o = 425$ mM, $[HCO_3^-]_o = 12$ mM). The $K_m$ (Na) was 71 ± 12 mM, which is not significantly different from the value of 77 ± 12 mM previously obtained on intact axons (Boron and Russell, 1983). Although the $J_{max}$ obtained by varying $[Na^+]_o$ at 12 mM $[HCO_3^-]_o$ (i.e., 17.8 ± 3.0 pmol·cm$^{-2}$·s$^{-1}$) is not significantly different from that obtained by varying $[HCO_3^-]_o$ at 425 mM $[Na^+]_o$ (18.6 ± 1.2 pmol·cm$^{-2}$·s$^{-1}$), it exceeds that previously obtained in intact axons (i.e., 10.3 ±
TABLE I

Dependences of Acid Extrusion on [HCO₃⁻]₀ at Three Levels of [Na⁺]₀.

<table>
<thead>
<tr>
<th>[Na⁺]₀ (mM)</th>
<th>Fit*</th>
<th>n</th>
<th>Apparent K_m (mM)</th>
<th>Apparent f_max (pmol·cm⁻²·s⁻¹)</th>
</tr>
</thead>
<tbody>
<tr>
<td>425</td>
<td>2</td>
<td>31</td>
<td>2.6±0.3</td>
<td>18.6±1.2</td>
</tr>
<tr>
<td>212</td>
<td>1</td>
<td>40</td>
<td>5.4±1.0</td>
<td>18.7±1.2</td>
</tr>
<tr>
<td>106</td>
<td>1</td>
<td>44</td>
<td>9.7±2.1</td>
<td>19.2±1.5</td>
</tr>
</tbody>
</table>

* Type 1 fit: standard Michaelis-Menten equation. Type 2: the fit is forced through a standard point ([HCO₃⁻]₀ = 12 mM, fₘₐₓ = 15.8 pmol·cm⁻²·s⁻¹). n is the number of points fitted.

Figure 4. Dependence of acid extrusion rate (fₘₐₓ) on [Na⁺]₀ at three fixed levels of [HCO₃⁻]: 12 (●), 6 (○), and 3 mM (△). Data from experiments similar to that of Fig. 2 were fitted by nonlinear, least-squares methods. The curve for [HCO₃⁻]₀ = 12 mM (type 2 fit) was forced through the point corresponding to the composition of the standard solution (i.e., [Na⁺] = 425 mM, indicated by the asterisk). The [HCO₃⁻]₀ = 6 and 3 mM curves represent type 1 fits to the standard Michaelis-Menten equation. The vertical bars indicate standard errors. In the inset, the data are replotted in double-reciprocal form. The straight lines through these replotted data are drawn according to the same Kₘ and fₘₐₓ values used to construct the curved plots in the main part of the figure.
0.6) by a considerable amount. As noted above, the discrepancy is probably due to the higher [Cl⁻]i in the present study.

The data for [HCO₃]₀ values of 6 and 3 mM were first fitted to a standard Michaelis-Menten equation (type 1 fit). At an [HCO₃]₀ of 6 mM, the best-fit value for Kₘ (Na) was 174 ± 45 mM, 2.5-fold higher than that at 12 mM [HCO₃]₀ (see Table II, line 2, and Fig. 4, middle curve). Jₘₐₓ, on the other hand, was 18.4 ± 2.0 pmol·cm⁻²·s⁻¹, which is not significantly different from the value in 12 mM [HCO₃]₀. Reducing [HCO₃]₀ to 3 mM, one-fourth of its control value, increased Kₘ (Na) ~3.7-fold, to 261 ± 102 mM (Table II, line 3, and Fig. 4, lower curve). Although Jₘₐₓ decreased somewhat, to 15.4 ± 3.2 mM, it was not significantly different from the value in 12 mM [HCO₃]₀. The accuracy of this last type 1 fit is expected to be limited, however, because the increase in Kₘ (Na) could not be matched by a corresponding increase in the maximal [Na⁺]ᵢ tested in the experiments. I also fitted the 6 and 3 mM HCO₃ data to a modified Michaelis-Menten equation in which Jₘₐₓ was predetermined (type 3 fit; see Methods). The chosen Jₘₐₓ was 18.6 pmol·cm⁻²·s⁻¹, the value obtained by fitting all the data of this study as a function of [NaCO₃]₀ (see below). This type 3 fit (Table II, line 5) resulted in approximately the same Kₘ values, but with substantially lower standard deviations. At 3 mM [HCO₃]₀, Kₘ (Na) was 364 ± 34 mM, ~5.1-fold greater than in 12 mM [HCO₃]₀. For the data in 6 mM [HCO₃]₀, the type 5 fit (Table II, line 4) yielded a Kₘ (Na) of 179 ± 15 mM, which is not very different from the value produced by the type 1 fit. In summary, the data of Table II are consistent with the NaCO₃ ion-pair model (see Discussion), which predicts that Kₘ (Na) should be inversely proportional to [HCO₃]₀, whereas Jₘₐₓ should be independent of [HCO₃]₀.

**DISCUSSION**

**Validity of Approach**

The kinetic analysis of the data is greatly simplified if the JH values correspond to "initial" rates. One way this can be ensured in the present experiments is by removing internal Na⁺, which obviates a possible reversal of the pH₅-regulating mechanism. Although dialysis with a Na-free solution should reduce [Na⁺]ᵢ to

<table>
<thead>
<tr>
<th>[HCO₃]₀</th>
<th>Fit*</th>
<th>n</th>
<th>Apparent Kₘ (Na⁺)</th>
<th>Apparent Jₘₐₓ</th>
</tr>
</thead>
<tbody>
<tr>
<td>mM</td>
<td></td>
<td></td>
<td>mM</td>
<td>pmol·cm⁻²·s⁻¹</td>
</tr>
<tr>
<td>12</td>
<td>2</td>
<td>35</td>
<td>71±12</td>
<td>17.8±3.0</td>
</tr>
<tr>
<td>6</td>
<td>1</td>
<td>30</td>
<td>174±45</td>
<td>18.4±2.0</td>
</tr>
<tr>
<td>3</td>
<td>1</td>
<td>33</td>
<td>261±102</td>
<td>15.4±5.2</td>
</tr>
<tr>
<td>6</td>
<td>3</td>
<td>30</td>
<td>179±15</td>
<td>18.6</td>
</tr>
<tr>
<td>3</td>
<td>3</td>
<td>33</td>
<td>364±34</td>
<td>18.6</td>
</tr>
</tbody>
</table>

* Type 1 fit: standard Michaelis-Menten equation. Type 2: the fit is forced through a standard point. Type 3: Jₘₐₓ is preset to a lumped Jₘₐₓ value. n is the number of points fitted.
near-zero levels during the period of dialysis, \([\text{Na}^+]_i\) would be expected to rise after dialysis is halted. Although I have no data on \(\text{Na}^+\) influxes under the present experimental conditions (\(\text{pH}_i = 6.6\), \([\text{Cl}^-]_i = 400\ \text{mM}\)), an influx of 10 \(\text{pmol} \cdot \text{cm}^{-2} \cdot \text{s}^{-1}\) would cause \([\text{Na}^+]_i\) to rise by <3 mM/h. A significant reversal of the \(\text{pH}_i\)-regulating mechanism is unlikely even at \([\text{Na}^+]_i\) levels exceeding 100 mM, given my inability to demonstrate such a reversal despite considerable effort (unpublished observations).

The acid extrusion rate of the squid axon is sensitive to changes in \(\text{pH}_i\) and \([\text{Cl}^-]_i\). (Boron and Russell, 1983). As can be seen in column 5 of Table III, the groups of data in the present study were obtained at rather similar mean \(\text{pH}_i\)

<table>
<thead>
<tr>
<th>[NaCO₃]₀ μM</th>
<th>[Na⁺]₀ mM</th>
<th>[HCO₃]₀ mM</th>
<th>Acid extrusion rate pmol cm⁻² s⁻¹</th>
<th>Mean pHᵢ</th>
<th>n</th>
</tr>
</thead>
<tbody>
<tr>
<td>402</td>
<td>425</td>
<td>12</td>
<td>15.3±0.6</td>
<td>6.69±0.01</td>
<td>63</td>
</tr>
<tr>
<td>212</td>
<td>24</td>
<td>15.1±0.7</td>
<td>6.77±0.03</td>
<td>8</td>
<td></td>
</tr>
<tr>
<td>106</td>
<td>48</td>
<td>16.1±1.5</td>
<td>6.73±0.03</td>
<td>6</td>
<td></td>
</tr>
<tr>
<td>201</td>
<td>425</td>
<td>6</td>
<td>13.4±0.4</td>
<td>6.85±0.03</td>
<td>7</td>
</tr>
<tr>
<td>212</td>
<td>12</td>
<td>13.7±1.2</td>
<td>6.73±0.03</td>
<td>6</td>
<td></td>
</tr>
<tr>
<td>106</td>
<td>24</td>
<td>13.9±0.8</td>
<td>6.69±0.01</td>
<td>6</td>
<td></td>
</tr>
<tr>
<td>100.5</td>
<td>425</td>
<td>3</td>
<td>9.9±1.0</td>
<td>6.74±0.05</td>
<td>6</td>
</tr>
<tr>
<td>212</td>
<td>6</td>
<td>9.5±0.9</td>
<td>6.74±0.03</td>
<td>8</td>
<td></td>
</tr>
<tr>
<td>106</td>
<td>12</td>
<td>10.3±1.0</td>
<td>6.71±0.02</td>
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</tr>
<tr>
<td>50.3</td>
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<td>1.5</td>
<td>6.2±0.2</td>
<td>6.88±0.02</td>
<td>6</td>
</tr>
<tr>
<td>212</td>
<td>3</td>
<td>6.2±0.2</td>
<td>6.74±0.03</td>
<td>7</td>
<td></td>
</tr>
<tr>
<td>106</td>
<td>6</td>
<td>7.2±0.6</td>
<td>6.76±0.04</td>
<td>4</td>
<td></td>
</tr>
<tr>
<td>53</td>
<td>12</td>
<td>7.7±1.2</td>
<td>6.76±0.02</td>
<td>7</td>
<td></td>
</tr>
<tr>
<td>25.1</td>
<td>425</td>
<td>0.75</td>
<td>4.6±0.6</td>
<td>6.87±0.05</td>
<td>8</td>
</tr>
<tr>
<td>212</td>
<td>1.5</td>
<td>5.4±0.3</td>
<td>6.78±0.06</td>
<td>4</td>
<td></td>
</tr>
<tr>
<td>106</td>
<td>3</td>
<td>4.9±0.9</td>
<td>6.77±0.03</td>
<td>8</td>
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</tr>
<tr>
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<td>4.9±0.8</td>
<td>6.79±0.05</td>
<td>5</td>
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</tr>
<tr>
<td>26.5</td>
<td>12</td>
<td>5.2±0.7</td>
<td>6.76±0.02</td>
<td>8</td>
<td></td>
</tr>
<tr>
<td>12.6</td>
<td>212</td>
<td>0.75</td>
<td>2.4±0.3</td>
<td>6.77±0.07</td>
<td>7</td>
</tr>
<tr>
<td>106</td>
<td>1.5</td>
<td>2.6±0.7</td>
<td>6.81±0.05</td>
<td>5</td>
<td></td>
</tr>
<tr>
<td>53</td>
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<td>2.4±0.5</td>
<td>6.81±0.03</td>
<td>5</td>
<td></td>
</tr>
<tr>
<td>26.5</td>
<td>6</td>
<td>2.6±0.7</td>
<td>6.74±0.03</td>
<td>6</td>
<td></td>
</tr>
<tr>
<td>6.3</td>
<td>106</td>
<td>0.75</td>
<td>2.0±0.3</td>
<td>6.72±0.05</td>
<td>5</td>
</tr>
<tr>
<td>26.5</td>
<td>3</td>
<td>1.9±0.6</td>
<td>6.77±0.04</td>
<td>7</td>
<td></td>
</tr>
<tr>
<td>0.0</td>
<td>425</td>
<td>0</td>
<td>-0.4±0.4</td>
<td>6.95±0.04</td>
<td>4</td>
</tr>
<tr>
<td>0</td>
<td>12</td>
<td>-0.3±0.4</td>
<td>6.72±0.06</td>
<td>4</td>
<td></td>
</tr>
</tbody>
</table>

* Within any group, the differences between calculated acid extrusion rates are not statistically significant, as determined by the unpaired Student's \(t\) test.
values. Furthermore, the pH dependence of $J_H$ in squid axons apparently is not as great as in other cells. In barnacle muscle, for example, $J_H$ is $>10$ times as great at pH 6.8 as at pH 7.3 (Boron et al., 1979), whereas in squid axons, this factor is only $\sim 2$ (Boron and Russell, 1983). Thus, the error introduced by pH variability should be minimal. The axon's pH-regulating mechanism has a $K_m$ for internal Cl$^-$ of $\sim 84$ mM (Boron and Russell, 1983). Because the nominal [Cl$^-$] of 400 mM exceeded this by a factor of 4.7, it is unlikely that small shifts of [Cl$^-$] during an experiment could have seriously affected $J_H$. In one control experiment, [Na$^+$]o and [HCO$_3^-$]o were kept approximately constant (at 425 mM and 12 mM, respectively), while I mimicked a normal sequence of solution changes. That is, four solutions were delivered from individual syringes, and pH was allowed to rise over its normal range. The values of $J_H$ for the four solutions were indistinguishable, which confirmed my suspicion that small pH changes as well as possible variations in [Cl$^-$]o or [Na$^+$]o had a negligible effect on the results.

Kinetic Models of Acid Extrusion

The data of Figs. 3 and 4 can be analyzed in terms of several kinetic models. In the following discussion, I specifically consider the ion-pair hypothesis (Fig. 1D) and the Na$^+$ plus CO$_3^-$ hypothesis (Fig. 1C). The latter actually includes three kinetically distinct models: (a) the random binding of Na$^+$ and CO$_3^-$, (b) the ordered binding of Na$^+$ and then CO$_3^-$, and (c) the ordered binding of CO$_3^-$ and then Na$^+$. Because [HCO$_3^-$] is proportional to [CO$_3^-$] at constant pH, these three models dealing with Na$^+$ plus CO$_3^-$ (Fig. 1C) apply equally well to models involving the binding of Na$^+$ plus a single HCO$_3^-$ (Fig. 1A). In addition, these three analyses could also apply to the binding of Na$^+$ and two HCO$_3^-$ (Fig. 1B), provided the binding of the two HCO$_3^-$ is governed by sufficiently different equilibrium constants. Thus, the following discussion applies to models A, C, and D of Fig. 1, and may apply to model B.

**THE NaCO$_3^-$ ION-PAIR MODEL**

The ion-pair hypothesis (Fig. 1D) predicts that $J_H$ should be determined by [NaCO$_3^-$]o, which is proportional (at fixed pH$_o$) to the product [Na$^+$]o·[HCO$_3^-$]o, and not by [Na$^+$]o or [HCO$_3^-$]o per se. The NaCO$_3^-$ model predicts the following values for apparent $K_m$ (Na) and $J_{max}$ (Na):

$$K_m \ (Na) = \frac{\gamma K_m [H^+]_o}{[HCO_3^-(o)}}$$

and

$$J_{max} \ (Na) = J_{max},$$

where $K_m$ is the true $K_m$ for external NaCO$_3^-$, $J_{max}$ is the true $J_{max}$ and $\gamma = ([Na^+]_o·[HCO_3^-])/([NaCO_3^-]·[H^+])$. Similarly, for the apparent $K_m$ (HCO$_3^-$) and $J_{max}$ (HCO$_3^-$) values:

$$K_m \ (HCO_3^-) = \frac{\gamma K_m [H^+]_o}{[Na^+]_o}$$

and

$$J_{max} \ (HCO_3^-) = J_{max}.$$
In other words, the apparent $K_m$ values for $\text{Na}^+$ and $\text{HCO}_3^-$ should be inversely proportional to the concentration of the opposite ion, and the $J_{\text{max}}$ values should be independent of either $[\text{Na}^+]_o$ or $[\text{HCO}_3^-]_o$. Within experimental error, these predictions have been verified by the present data. Another expression of these kinetic predictions is that if the $J_H$ data are plotted as a function of $[\text{Na}\text{CO}_3]_o$, they should all fall along the same Michaelis-Menten curve, regardless of the particular values of $[\text{Na}^+]_o$ or $[\text{HCO}_3^-]_o$ used to achieve the $[\text{Na}\text{CO}_3]_o$. Fig. 5 is a replot of all the $J_H$ data of this study as a function of $[\text{Na}\text{CO}_3]_o$, the latter calculated from $[\text{Na}^+]_o$, $[\text{HCO}_3^-]_o$, and $\text{pH}_o$ according to the stability constant data of Garrels et al. (1961).

![Figure 5](image)

**Figure 5.** Dependence of acid extrusion rate on the calculated $[\text{Na}\text{CO}_3]_o$. The data from Figs. 3 and 4 are replotted as a function of $[\text{Na}\text{CO}_3]_o$, calculated from $[\text{Na}^+]_o$, $[\text{HCO}_3^-]_o$, and $\text{pH}_o$ ($\text{pH}_o = 8.0$) according to the stability constant data of Garrels et al. (1961). It is clear that, within experimental error, all the data fall along the same Michaelis-Menten curve, which was drawn from best-fit values of $80 \pm 8 \mu\text{M}$ for $K_m$ ($[\text{Na}\text{CO}_3]$) and $18.6 \pm 0.7 \text{ pmol}\cdot\text{cm}^{-2}\cdot\text{s}^{-1}$ for $J_{\text{max}}$. These data are also presented in Table III, which shows that for any value of $[\text{Na}\text{CO}_3]_o$, there is no significant difference among $J_H$ values obtained with different combinations of $[\text{Na}^+]_o$ and $[\text{HCO}_3^-]_o$. The present data are thus fully consistent with the ion-pair model.

**Random Binding of $\text{Na}^+$ and $\text{CO}_3^-$** If $\text{Na}^+$ and $\text{CO}_3^-$ (Fig. 1C) bind randomly to the transporters, and if the binding of each ion is rapid compared with the transport step, then the transport process can be described by the following...
reaction sequence:

\[ \begin{align*}
X + Na & \xrightarrow{K_{Na}} X \cdot Na \\
+ & \quad + \\
CO_3 & \quad CO_3 \\
\| K_c & \quad \| aK_c \\
X \cdot CO_3 + Na & \xrightarrow{aK_{Na}} X \cdot Na \cdot CO_3 \end{align*} \]

where \( X \) is the transporter, \( K_{Na} \) and \( K_c \) are equilibrium constants, \( k \) is the rate constant of the slow transport step across the membrane, and \( a \) is the factor by which the equilibrium constant for the binding of one substrate is altered by the binding of the other substrate. Thus, when \( a = 1 \), the affinity of the transporter for one substrate is unaffected by the binding of the other substrate, whereas if \( a \) falls below 1, the affinity is increased by the binding of the other substrate. The assumptions of rapid-equilibrium kinetics lead to the following predictions for the apparent \( J_{max} \) and the apparent \( K_m \) when \([Na^+]_o\) is varied at fixed \([CO_3^-]_o\) (i.e., at fixed pH and \([HCO_3^-]_o\)):

\[
K_m (Na) = \frac{aK_c + a[CO_3^-]}{\alpha K_c + [CO_3^-]} K_{Na},
\]

and

\[
J_{max} (Na) = \frac{[CO_3^-]}{[CO_3^-] + aK_c} J_{max},
\]

where \( J_{max} \) is the true maximal velocity for the reaction. Similarly, when \([CO_3^-]_o\) is varied at fixed \([Na^+]_o\):

\[
K_m (CO_3) = \frac{aK_{Na} + a[Na^+]}{\alpha K_{Na} + [Na^+]} K_c,
\]

and

\[
J_{max} (CO_3) = \frac{[Na^+]}{[Na^+] + aK_{Na}} J_{max}.
\]

The kinetic predictions of this and several other models are given in Table IV, along with the experimental observations. To minimize the bias, only the results of type 1 and type 2 fits are included in Table IV. Inasmuch as \([HCO_3^-]\) is proportional to \([CO_3^-]\) at constant pH, I will refer to \( HCO_3^- \) as the independent variable. The \( K_m (HCO_3^-) \) and \( J_{max} (HCO_3^-) \) values at 212 and 106 mM \( Na^+ \) are given relative to the values in 425 mM \( Na^+ \) (assumed to be unity). Conversely, \( K_m (Na^+) \) and \( J_{max} (Na^+) \) values at 6 and 3 mM \( HCO_3^- \) are given relative to the values at 12 mM \( HCO_3^- \). The predicted values that fall >2 SD from the observed value are given in parentheses. The predictions of the rapid-equilibrium, random-binding model depend on the value chosen for \( a \). For an \( a \) of unity (Table IV, line 1), the predicted \( K_m \) values are independent of the concentration of the
alternative substrate, whereas the predicted $J_{\text{max}}$ values vary by modest amounts. The predicted invariability of the $K_m$ values is clearly at odds with the data (compare lines 1 and 8). Even the predicted, modest changes in $J_{\text{max}}$ (HCO$_3^-$) are $>2$ SD away from the negligible changes observed. Although the predicted $J_{\text{max}}$ (Na) values are within $2$ SD of the observed ones, this is probably the fortuitous consequence of the large standard deviations of the curve-fitted (i.e., experimental) values.$^1$

If the assumed $\alpha$ is lowered to 0.5 or to 0.1, the predicted $K_m$ and $J_{\text{max}}$ values still fall $>2$ SD from the observed values, although the discrepancy is smaller. If $\alpha$ is zero, however, the kinetic predictions of the random-binding model are exactly the same as those of the ion-pair model. I therefore cannot rule out a rapid-equilibrium, random-binding model$^2$ if $\alpha$ is sufficiently close to zero. An $\alpha$ of zero implies that once the transporter binds one substrate, it has an infinite affinity for (i.e., automatically binds) the other substrate. Thus, for all practical purposes, the case in which $\alpha$ approaches zero is kinetically indistinguishable from the ion-pair model. It is theoretically distinct, however, inasmuch as the binding of Na$^+$ and CO$_3^{2-}$ to separate sites would be quite different mechanistically from the binding of a NaCO$_3$ to a single site.

If the binding of Na$^+$ and CO$_3^{2-}$ (or HCO$_3^-$) is not rapid compared with the transport step, the assumptions of rapid-equilibrium kinetics are not valid, and

TABLE IV
Predictions of Rapid-Equilibrium Kinetic Models

<table>
<thead>
<tr>
<th>$K_m$ (Na)</th>
<th>$J_{\text{max}}$ (Na)</th>
<th>$K_m$ (HCO$_3^-$)</th>
<th>$J_{\text{max}}$ (HCO$_3^-$)</th>
</tr>
</thead>
<tbody>
<tr>
<td>[HCO$_3^-$], mM</td>
<td>[Na$^+$], mM</td>
<td>[HCO$_3^-$], mM</td>
<td>[Na$^+$], mM</td>
</tr>
<tr>
<td>12</td>
<td>6</td>
<td>5</td>
<td>12</td>
</tr>
<tr>
<td>(1) Random Na$^+$ and CO$_3^{2-}$, $\alpha = 1$</td>
<td>1.00</td>
<td>(1.00)</td>
<td>(1.00)</td>
</tr>
<tr>
<td>(2) Random Na$^+$ and CO$_3^{2-}$, $\alpha = 0.5$</td>
<td>1.00</td>
<td>(1.07)</td>
<td>(1.19)</td>
</tr>
<tr>
<td>(3) Random Na$^+$ and CO$_3^{2-}$, $\alpha = 0.1$</td>
<td>1.00</td>
<td>(1.15)</td>
<td>(1.44)</td>
</tr>
<tr>
<td>(4) Random Na$^+$ and CO$_3^{2-}$, $\alpha = 0.0$</td>
<td>1.00</td>
<td>2.00</td>
<td>4.00</td>
</tr>
<tr>
<td>(5) Ordered, Na$^+$ then CO$_3^{2-}$</td>
<td>1.00</td>
<td>1.70</td>
<td>2.61</td>
</tr>
<tr>
<td>(6) Ordered, CO$_3^{2-}$ then Na$^+$</td>
<td>1.00</td>
<td>(1.18)</td>
<td>(1.53)</td>
</tr>
<tr>
<td>(7) NaCO$_3$</td>
<td>1.00</td>
<td>2.00</td>
<td>4.00</td>
</tr>
<tr>
<td>(8) Observed</td>
<td>1.00</td>
<td>2.45</td>
<td>5.68</td>
</tr>
</tbody>
</table>

$^1$ The observed (i.e., fitted) values for $K_m$ (Na) and $J_{\text{max}}$ (Na) have anomalously high standard deviations for [HCO$_3^-$] = 6 mM, and especially for [HCO$_3^-$] = 3 mM. These parameters, the result of type 1 curve fits, can be determined only with limited accuracy when [Na$^+$], cannot be raised sufficiently to have $J$ approach $J_{\text{max}}$.

$^2$ Because [HCO$_3^-$] is proportional to [CO$_3^{2-}$] at constant pH, the predictions of any model for the binding of Na$^+$ and one HCO$_3^-$ are the same as those for Na$^+$ and CO$_3^{2-}$.
the data must be analyzed by the much more complex "steady state" approach (Segal, 1975). Although I have not attempted such an analysis, there are two reasons why it is likely that a set of rate constants could be found for which a steady state, random-binding model could account for the data. First, the rapid-equilibrium approach can account for the data as \( \alpha \) approaches zero, and the steady state approach is even more general. Second, as noted below, the two ordered-binding, steady state models can account for the data, and the random-binding model is even more general.

**ORDERED BINDING OF Na\(^{+}\) AND CO\(_{3}^{2-}\)** If Na\(^{+}\) and then CO\(_{3}^{2-}\) (Fig. 1C) bind to the transporter, and if these binding steps are rapid compared with the transport step, the overall transport process can be described by the following reaction sequence:

\[
X + Na \xrightleftharpoons[K_{Na}]{K_{c}} X \cdot Na + CO_3
\]

The assumptions of rapid-equilibrium kinetics lead to the following predictions for the apparent \( K_m \) and \( J_{max} \) values:

\[
K_m (Na) = \frac{K_c}{K_c + [CO_3^{2-}]} K_{Na},
\]

\[
J_{max} (Na) = \frac{[CO_3^{2-}]}{K_c + [CO_3^{2-}]} J_{max},
\]

and

\[
K_m (CO_3) = \frac{[Na^{+}] + K_{Na}}{[Na^{+}]} K_c,
\]

\[
J_{max} (CO_3) = J_{max}.
\]

The predicted \( K_m \) and \( J_{max} \) values for this model are given in Table IV, line 5. The predicted \( J_{max} \) values\(^1\) as well as the \( K_m \) (Na) values, are within 2 SD of the observations. However, the predicted values of \( K_m \) (HCO\(_{3}^{-}\)) are substantially less than those observed, allowing us to rule out the rapid-equilibrium, ordered binding of \( Na^{+} \) then CO\(_{3}^{2-}\) (or HCO\(_{3}^{-}\)) for the squid axons.\(^2\)

If the binding of \( Na^{+} \) and CO\(_{3}^{2-}\) (or HCO\(_{3}^{-}\)) is not rapid compared with the transport step, then the more general approach of steady state kinetics must be applied. Sanders et al. (1984) have analyzed the kinetic predictions of an ordered-binding cotransport model for a variety of boundary conditions. Their analysis of the "zero trans-ligand" boundary condition (analogous to \( [Na^{+}]_i = 0 \) in my experiments) shows that for a restricted combination of rate constants (see their Table II, column 2, rows 9 and 10), the ordered binding of \( Na^{+} \) and CO\(_{3}^{2-}\) (or
HCO$_3^-$ can account for my data. The reverse order of binding (i.e., CO$_2^-$ or HCO$_3^-$, then Na$^+$) can also account for my data, given a similarly restricted combination of rate constants.

**ORDERED BINDING OF CO$_2^-$ AND Na$^+$** If CO$_2^-$ and then Na$^+$ (Fig. 1 C) bind to the transporter, and if these binding steps are rapid compared with the transport step, the overall transport process can be described by the following reaction sequence:

$$X + CO_3 \xrightarrow{K_c} X \cdot CO_3$$

The assumptions of rapid-equilibrium kinetics lead to the following predictions for apparent $K_m$ and $J_{max}$ values:

$$K_m (Na) = \frac{[CO_3^2-] + K_c}{[CO_3^2-]} K_{Na},$$

$$J_{max} (Na) = J_{max},$$

$$K_m (CO_3) = \frac{K_{Na}}{K_{Na} + [Na^+] K_c},$$

and

$$J_{max} (CO_3) = \frac{[Na^+]}{K_{Na} + [Na^+]} J_{max}.$$
Comparison with the pH-regulating System of Barnacle Muscle

As noted in the Introduction, a similar though less complete kinetic study of the pH-regulating system in the barnacle muscle fiber (Boron et al., 1981) yielded data inconsistent with the ion-pair model. Specifically, when the \([\text{Na}^+]_0\) dependence was examined at two different \([\text{HCO}_3^-]_0\) values (at a constant \(\text{pH}_e\) of 8.0), there were only slight effects on \(K_m (\text{Na})\), but there was a substantial change in \(J_{\text{max}} (\text{Na})\). This is the opposite of the pattern observed in the present experiments and the opposite of that predicted by the ion-pair model. More recently, A. Roos and T. J. Wilding (unpublished observations) have studied the \([\text{HCO}_3^-]_0\) dependence of acid extrusion at external \(\text{Na}^+\) concentrations of 440 and 40 mM in barnacle muscle. They found that altering \([\text{Na}^+]_0\) has a major effect on \(J_{\text{max}} (\text{HCO}_3^-)\), and only small effects on \(K_m (\text{HCO}_3^-)\). These results are compatible with those previously obtained on barnacle muscle (Boron et al., 1981), and again indicate that the ion-pair hypothesis cannot account for pH regulation in that preparation. It thus appears that there is a consistent difference between the kinetics of the pH regulator in barnacle muscle and squid axons: the barnacle data are consistently irreconcilable with the ion-pair model, whereas the squid data are consistently supportive of this model. These kinetic differences are not the first discrepancies between the pH regulators of these two preparations. The barnacle muscle's transporter is easily reversible (Russell et al., 1983), is stimulated by cyclic AMP (Boron et al., 1978), and is supported by \(\text{Li}^+\) nearly as well as by \(\text{Na}^+\) (Boron et al., 1981). The squid axon's transporter, on the other hand, has not been reversed despite considerable effort (unpublished observations), is not stimulated by cyclic AMP (Russell, J. M., and W. F. Boron, unpublished observations), and is not supported by \(\text{Li}^+\) (Boron and Russell, 1983). Thus, although the pH-regulating systems superficially appear similar in squid axons and barnacle muscle, there are several more subtle differences between them.

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